

**Please cite the Published Version**

Parr, Johnny VV, Wright, David J, Uiga, Liis, Marshall, Ben, Mohamed, Mohamed Omar and Wood, Greg (2022) A scoping review of the application of motor learning principles to optimize myoelectric prosthetic hand control. *Prosthetics and Orthotics International*, 46 (3). pp. 274-281. ISSN 0309-3646

**DOI:** <https://doi.org/10.1097/pxr.0000000000000083>

**Publisher:** Lippincott, Williams & Wilkins

**Version:** Accepted Version

**Downloaded from:** <https://e-space.mmu.ac.uk/628913/>

**Usage rights:** © In Copyright

**Additional Information:** This is an Author Accepted Manuscript of an article published in *Prosthetics and Orthotics International*.

**Enquiries:**

If you have questions about this document, contact [openresearch@mmu.ac.uk](mailto:openresearch@mmu.ac.uk). Please include the URL of the record in e-space. If you believe that your, or a third party's rights have been compromised through this document please see our Take Down policy (available from <https://www.mmu.ac.uk/library/using-the-library/policies-and-guidelines>)



31 **Abstract**

32 Although prosthetic hand rejection rates remain high, evidence suggests that effective training plays a  
33 major role in device acceptance. Receiving training early in the rehabilitation process also enhances  
34 functional prosthetic use, decreases the likelihood of developing an over-reliance on the intact limb  
35 and reduces amputation-related pain. Despite these obvious benefits, there is a current lack of  
36 evidence regarding the most effective training techniques to facilitate myoelectric prosthetic hand  
37 control and it remains unknown whether training is effective in facilitating the acquisition and transfer  
38 of prosthetic skill. In this scoping review, we introduce and summarise key motor learning principles  
39 related to attentional focus, implicit motor learning, training eye-hand coordination, practice  
40 variability, motor imagery and action observation, and virtual training and biofeedback. We then  
41 review the existing literature that has applied these principles for training prosthetic hand control  
42 before outlining future avenues for further research. The importance of optimising early and  
43 appropriate training cannot be overlooked. While the intuition and experience of clinicians holds  
44 enormous value, evidence-based guidelines based on well-established motor learning principles will  
45 also be crucial for training effective prosthetic hand control. While it is clear that more research is  
46 needed to form the basis of such guidelines, it is hoped that this review highlights the potential  
47 avenues for this work.

48 **Keywords:** *training; rehabilitation; motor control; motor learning; prosthesis rejection.*

49

50

51

52

53

54

55

## 56 1. Introduction

57 Recent evidence suggests that prosthetic hand rejection rates are as high as 44%<sup>1</sup>, although  
58 reported rates appear to vary considerably<sup>2,3</sup>. This is concerning, as amputees who do not use their  
59 prosthesis report more difficulty performing activities of daily living, greater overall disability, and  
60 lower physical function compared to amputees who choose to use their prosthesis frequently<sup>3</sup>. Those  
61 who reject their prosthesis also exhibit an over-reliance on the intact side of their body that often leads  
62 to overuse injuries<sup>4</sup>. The factors contributing to prosthesis abandonment are numerous, with users  
63 consistently reporting dissatisfaction with prosthesis appearance, weight, comfort, and fitting<sup>1,5,6</sup>.  
64 However, a major contributor seems to be related to the poor functionality of these devices and the  
65 difficulty users have experienced in learning to control them to interact successfully with their  
66 environment<sup>5,7</sup>. To tackle this, efforts have been placed upon developing prosthesis technologies to  
67 improve intuitive control through additional sensory feedback mechanisms<sup>8</sup> and EMG pattern  
68 recognition<sup>9</sup>. However, these technological efforts might be in vain for most of the intended population  
69 given the high cost associated with these systems. This is especially true for children, who may  
70 frequently require new prostheses and/or modifications to accommodate for growth and damage.

71 There is strong evidence to suggest that prosthesis training plays a major role in device  
72 acceptance. Early specialised training enhances functional prosthetic use<sup>10</sup>, decreases the likelihood of  
73 developing an over-reliance on the intact limb<sup>11</sup>, and even reduces amputation-related pain<sup>12</sup>. Receiving  
74 adequate training is also linked with higher levels of both physical and mental health, suggesting that  
75 early intervention can have long-term effects on overall quality of life<sup>3</sup>. However, prosthesis users  
76 commonly report dissatisfaction with the training they receive to help them learn to control their device<sup>5</sup>  
77 and/or feel that their training did not sufficiently meet their needs<sup>13</sup>. This is important as user perceptions  
78 that the training received is *useful* is more closely aligned with prosthesis acceptance than the overall  
79 amount of training received<sup>1</sup>. The need to develop quality, well-designed, and patient-tailored training  
80 protocols has therefore been highlighted as a priority by users<sup>5</sup> and a clinical imperative to increasing  
81 long-term prosthesis use and acceptance<sup>1,3</sup>.

82 Current prosthetic training programmes are clinic-specific, with rehabilitation centres often  
83 using their own, locally developed protocols that are based on intuition and clinical experience<sup>10,14</sup>.  
84 Consequently, the training a patient receives is likely to differ due to the varying experience levels of  
85 prosthetists and therapists. Due to the current lack of evidence regarding the most effective training  
86 techniques to facilitate myoelectric prosthetic hand control, it is unknown whether training is efficient  
87 or effective in facilitating the acquisition and transfer of prosthetic skills<sup>15</sup>. Researchers have therefore  
88 been advocating for the development of evidence-based training protocols for some time<sup>16</sup>, with the  
89 goal of maximising the efficiency, effectiveness, and consistency of rehabilitation. Yet, the extant  
90 literature dedicated to applying established motor learning principles to prosthetic hand skill acquisition  
91 and transfer remains sparse, with many fundamental components of rehabilitation underexplored. It is,  
92 therefore, the aim of this paper to review the current literature-base dedicated to understanding the  
93 motor learning principles that might contribute to the effectiveness of prosthetic hand learning and  
94 transfer. We will begin this paper by addressing key motor learning principles in a section-by-section  
95 manner, highlighting the relevant upper-limb prosthesis literature, and suggesting future research  
96 agendas based on established evidence-based methods from the fields of human movement, sport, and  
97 rehabilitation.

### 98 **3.1. Focus of attention**

99 The stress and frustration around learning or relearning to move effectively can cause learners  
100 to direct their focus internally and consciously attend to *how* they are moving. For example, stroke  
101 patients report a higher propensity to consciously monitor aspects of their movements compared to age-  
102 matched controls<sup>17</sup>, whilst people with Parkinson's disease increase their propensity to consciously  
103 monitor aspects of their movement over time<sup>18</sup>. Although no research has directly examined the extent  
104 to which prosthesis users focus internally, users have described their device as a "conscious burden"  
105 and are highly dependent on vision to monitor their prosthetic hand during movement<sup>19</sup>.

106 An extensive body of research has shown that adopting an internal focus of attention, compared  
107 to an external focus of attention, is less effective for motor performance and learning<sup>20</sup>. Whilst an  
108 internal focus occurs when an individual directs their attention towards bodily movements and/or

109 sensations, an external focus occurs when an individual instead directs their attention towards the  
110 outcomes of the movement or the effect the movement has upon the environment. For example, a  
111 prosthesis user could either be instructed to focus on “contracting the muscles of the residual limb” (i.e.,  
112 internal focus) or to simply focus on “closing the prosthesis” (i.e., external focus) when attempting to  
113 grasp an object. By focusing internally (contracting the muscles) it is proposed that the motor system  
114 becomes “constrained” and automatic control processes become disrupted, placing greater demands on  
115 working memory and attentional resources<sup>21</sup>. By contrast, focusing externally on the effect of movement  
116 (the closing of the prosthesis around an object) allows the motor system to self-organise uninhibited by  
117 conscious control. Supporting evidence from the sport and human movement literature has shown that  
118 an external focus enhances movement accuracy<sup>22</sup>, balance performance<sup>23</sup>, maximum vertical jump  
119 height<sup>24</sup> and maximum force production<sup>25</sup>, compared to an internal focus.

120         Despite the apparent advantage of an external focus of attention, it has recently been suggested  
121 that conventional prosthesis training mostly promotes an internal focus, with feedback and coaching  
122 typically centred on the muscular contractions rather than the actuation of the prosthesis resulting from  
123 said contractions<sup>26,27</sup>. It is, therefore, possible that current prosthesis training might be contributing to  
124 the difficulty users report controlling their device, especially when considering evidence that internal  
125 focus instructions might be less effective than receiving no instructions at all<sup>28</sup>. Indeed, an internal focus  
126 of attention appears to disrupt electromyographic (EMG) efficiency, increasing joint stiffness through  
127 co-contraction of antagonistic muscle pairs<sup>29,30</sup> and increasing the time to fatigue<sup>30</sup>. On a  
128 neurophysiological level, an internal focus appears to disrupt “surround inhibition” in the motor cortex,  
129 decreasing the contrast between task-relevant and task-irrelevant motor neurons leading to unnecessary  
130 contractions of muscles that are not directly involved in the task<sup>31,32</sup>. Given that fine prosthesis control  
131 is dependent on the generation of accurate EMG signals, promoting an internal focus may directly  
132 disrupt the effectiveness and efficiency of muscular activation and thus hinder prosthesis myocontrol.

133         Whilst attentional focus remains sparsely investigated in prosthesis control, some researchers  
134 have attempted to exploit the benefits of an external focus by employing “serious gaming”<sup>26,27</sup> to aid  
135 pattern recognition prosthesis control, and “gaze training”<sup>19</sup> to improve hand-eye coordination (see

136 section 2.3). Although both strategies have shown some advantages over more “conventional” training,  
137 any clear advantage has thus far been limited to able-bodied prosthesis users. Evidently, far greater  
138 work is needed to clarify (a) the attentional focus strategies employed by upper-limb prosthesis users,  
139 (b) how these strategies are promoted through current training protocols, (c) how attentional focus  
140 affects prosthesis performance and functionality, and (d) the potential benefits of promoting an external  
141 focus.

### 142 **3.2. Implicit Motor Learning**

143 For a prosthetic hand user, a simple activity like eating in public may be a source of anxiety,  
144 resulting in an increased internal focus and conscious control in an attempt to ensure desired movement  
145 outcomes. Thus, motor learning strategies that reduce the reliance on conscious processes might benefit  
146 prosthesis users. Implicit motor learning, an established alternative to more traditional (explicit) forms  
147 of motor learning, aims to reduce the amount of consciously accessible (declarative) task-relevant  
148 knowledge<sup>33</sup>. It is argued that learning motor skills explicitly, often through verbally conveyed task  
149 rules (such as technique instructions), encourages conscious processing as learners can apply acquired  
150 declarative knowledge to the online control of movements<sup>34</sup>. By bypassing the provision of declarative  
151 knowledge via implicit motor learning methods, skills can be developed without conscious thought,  
152 lowering demands on working memory and freeing up attentional resources for other tasks<sup>35</sup>. The  
153 benefits of implicit motor learning include robust performance under pressure, fatigue, and  
154 multitasking<sup>36-38</sup>. Furthermore, research has shown that implicit motor learning occurs independent of  
155 age, and cognitive and motor impairment<sup>39,40</sup>.

156 To our knowledge, there is currently little-to-no research directly investigating the potential  
157 benefit of implicit motor learning for upper-limb prosthesis skill acquisition. This is surprising, given  
158 the availability of many distinct strategies that can be used to exploit the proposed benefits of implicit  
159 learning. For example, error-reduced practice is proposed to encourage implicit learning by decreasing  
160 the amount of outcome errors made during skill acquisition, especially during the early stages of  
161 learning<sup>37</sup>. Commonly, error-reduced interventions start with an easily achievable task that is  
162 incrementally made more difficult throughout practice. For example, a prosthesis user could spend

163 considerable time grasping large malleable objects (e.g., sponge ball) before attempting more precise  
164 grasping actions (e.g., picking up coins). By minimising errors, it is argued that learners are less likely  
165 to engage in active hypothesis testing in search for alternative movement solutions, lowering cognitive  
166 effort and mitigating the accumulation of declarative knowledge<sup>37</sup>. Error-reduced practice has  
167 increasingly been employed in rehabilitation, showing benefits among Parkinson's disease patients<sup>41</sup>,  
168 stroke patients<sup>42</sup>, Alzheimer's disease patients<sup>43</sup>, and children with cerebral palsy<sup>44</sup>. Interestingly, error-  
169 reduced learning has also been shown to enhance the acquisition of prosthetic limb fitting skills in  
170 lower-limb amputees compared to typical (trial and error) treatment<sup>45</sup>. Error-reduced practice can also  
171 result in performance that is stable under physiological fatigue<sup>38</sup> and robust to secondary task loading<sup>37</sup>.  
172 Evidently, reducing errors during the initial stages of practice appears an effective implicit motor  
173 learning strategy that warrants more direct application to upper-limb prosthesis rehabilitation.

174         Implicit motor learning can also be achieved through the provision of a motor analogy  
175 instruction<sup>46</sup>. A motor analogy instruction has been described as an "all encompassing, biomechanical  
176 metaphor" that contains all the relevant information about the to-be-learned movement<sup>47</sup>. In this  
177 manner, familiarity with a concept in one domain (e.g., a right-angle triangle) can be used to disguise  
178 and facilitate the understanding of explicit rules within another domain<sup>46</sup> (e.g., the movement required  
179 to achieve a top spin forehand in table tennis). Thus, the new movement can be acquired with minimal  
180 load on declarative knowledge and information processing resources, leading to stable performance  
181 under pressure<sup>48</sup> and when having to make concurrent complex decisions<sup>49</sup>. Like error-reduced practice,  
182 motor analogy instructions have been increasingly used in rehabilitation<sup>50</sup>. For example, Jie et al.<sup>51</sup>  
183 instructed Parkinson's disease patients to pretend they were 'following footprints in the sand' during  
184 their everyday walking. Jie et al. found that clinically significant improvements for walking velocity  
185 were evident following analogy training. Furthermore, participants were able to perform a concurrent  
186 secondary task (both cognitive and motor) without affecting walking ability. The authors argued that  
187 successful dual-task performance demonstrates a potential transferability of motor analogy learning to  
188 activities of daily living.



189           A significant part of rehabilitation for prosthesis users focuses on improving functional ability  
190 by (re)learning activities of daily living. Implicit motor learning strategies, which place less demand on  
191 cognitive processes, and are more robust under pressure, might complement or even provide better  
192 alternatives to more traditional motor learning approaches. It is yet to be established whether implicit  
193 motor learning facilitates performance among prosthetic hand users, however, the implications for  
194 rehabilitation are promising.

### 195           **3.3. Hand-eye coordination and the utility of gaze training**

196           A commonly cited reason for prosthesis rejection is the high cognitive burden imposed on users  
197 to visually monitor ongoing actions to accommodate for the severe reductions in hand-related sensory  
198 feedback. Indeed, prosthetic hand users display a high tendency to watch the hand or objects being  
199 manipulated by the hand<sup>19,52,53</sup>, a behaviour rarely observed during able-bodied reaching and grasping  
200 <sup>54</sup>. The tendency to watch the hand is typically associated with an initial stage of learning, where vision  
201 is used to check the consequences of actions so that errors can be identified and corrected online<sup>55</sup>. With  
202 increasing skill, however, learners can typically better predict the consequences of their actions,  
203 allowing vision to retrieve feedforward (i.e., look at the object to be grasped) rather than a feedback  
204 (i.e., look at the hand when reaching for the object) information, as observed in typical anatomic hand  
205 control. These skill-related changes in visuomotor behaviours have been observed when learning to use  
206 laparoscopic surgical tools<sup>56</sup> and chopsticks<sup>57</sup>, with skilled behaviour seemingly underpinned by an  
207 increased ratio of target-related (feedforward) compared to tool-related (feedback) fixations. It would  
208 therefore be reasonable to assume that (a) the demands on the visual system to monitor prosthesis  
209 control would naturally decrease with experience, and that (b) gaze behaviour could be used to  
210 determine the skill level of prosthesis users and thus the degree of device integration. However,  
211 evidence thus far has failed to support these assumptions, with gaze strategies among experienced  
212 prosthesis users highly variable and seemingly unrelated to prosthesis functionality<sup>16</sup> or usage in the  
213 real-world<sup>53</sup>. Why, then, does the typical relationship between skill level and hand (tool) focused gaze  
214 not arise in prosthesis users as it does in other human-tool interactions (e.g., laparoscopy and  
215 chopsticks)?

216           One likely explanation is that prosthetic devices might be inherently too unpredictable to allow  
217 the development of reliable mapping rules. Unlike rigid ‘tools’ that have fixed intrinsic properties, the  
218 reliability of prosthesis responsiveness can fluctuate as a result of EMG signal artefact arising from  
219 sweating, poor fitting and/or fatigue<sup>58</sup>. Indeed, recent evidence has shown that prosthesis users who  
220 experience a greater frequency of undesired activations (hand accidentally opening/closing, no  
221 prosthesis response, or incorrect prosthesis response) during a shoulder flexion task are also more likely  
222 to exhibit decreased functionality and an increased time watching the prosthesis during a multi-stage  
223 functional task<sup>59</sup>. This tentatively suggests that the expectation of an undesired prosthesis response (i.e.,  
224 users do not trust their device) drives both poor performance and the over-reliance on gaze to visually  
225 monitor prosthesis control and safeguard against (the possibility of) task failure. Addressing the issue  
226 of prosthesis unpredictability could therefore be crucial to the development of effective prosthesis  
227 visuomotor control and the alleviation of cognitive resources dedicated to continuous prosthesis  
228 monitoring<sup>59</sup>.

229           Whilst the influence of prosthesis unpredictability cannot be overlooked, Parr et al. <sup>19</sup> provided  
230 evidence that the gaze strategies used to control a prosthesis can also be strongly influenced by the  
231 nature of training instructions. Specifically, Parr et al. administered one week of “gaze training”  
232 designed to encourage learners to adopt a “target focused” gaze strategy and avoid visually fixating the  
233 prosthesis, a method shown to expedite the acquisition of laparoscopic surgical skills<sup>60</sup>. Compared to a  
234 group who received explicit technique focused instructions (i.e., “movement training”), the gaze  
235 training group visually focused on the prosthesis less, completed the tasks quicker, and displayed more  
236 efficient brain activity (as indexed by electroencephalography; see<sup>61</sup>) at retention and delayed retention.

237           These findings have several potential implications for our understanding of the visuomotor  
238 control strategies observed in prosthesis users. For example, unless told otherwise, it appears that  
239 learners will maintain an overreliance on gaze to visually monitor prosthesis actions. As this behaviour  
240 has been observed in experienced prosthesis users, it likely reflects a compensatory behaviour to  
241 safeguard against task failure in the face of prosthesis unpredictability. However, the findings of Parr  
242 et al. suggest that this behaviour is not a prerequisite of prosthesis control, and users can be encouraged

243 to relinquish their reliance on vision to control movement. By doing so, users may become more  
244 proficient at utilising other “back-up” modalities of sensory information (e.g., auditory / proprioceptive  
245 feedback). It would therefore appear that prosthesis unpredictability might prevent the natural  
246 development of feedforward gaze control rather than the possibility of achieving it through intentional  
247 practice. Adopting feedforward gaze control also resulted in quicker movements and increased neural  
248 efficiency, possibly by encouraging an external focus of attention and bypassing the provision of  
249 explicit, movement-related instructions (i.e., implicit learning)<sup>19</sup>. Given that an internal focus of  
250 attention, and the tendency to consciously control motor actions, has been associated with less-effective  
251 and less-consistent myocontrol, it is important to recognise that prosthesis unpredictability might (to  
252 some extent) be user-driven by the cognitive strategies employed during prosthesis control.

### 253 **3.4. Practice variability and contextual interference**

254 Practice variability is a fundamental component of rehabilitation design. For example, if several  
255 prosthesis tasks must be learned within a single therapy session (e.g., different grip patterns), a learner  
256 could be asked to repetitively perform multiple trials of the same task (i.e., low variability) or to  
257 adaptively switch between different tasks or task variants on a trial-by-trial basis (i.e., high variability).  
258 Importantly, the Contextual Interference (CI) effect is a robust motor learning phenomenon that  
259 suggests the choice between either high or low practice variability is far from arbitrary and can have  
260 cascade effects on both immediate performance and long-term motor adaptation. Specifically, the CI  
261 effect states that practicing a “block” of repetitive trials of a single motor task before moving on to a  
262 new task (i.e., Blocked practice) facilitates performance during practice, but does not facilitate long-  
263 term learning. Conversely, constantly switching between different tasks in a random order (i.e., Random  
264 practice) increases performance error during practice (via task interference) but is more optimal for  
265 long-term motor adaptation at retention<sup>62,63</sup>. It is proposed that the frequent task switching imposed by  
266 a random schedule increases cognitive effort and thus memory consolidation<sup>64</sup>, supported by  
267 neurophysiological evidence that random practice elevates the activation of the cognitive, sensory, and  
268 motor regions of the brain<sup>65,66</sup>.

269           Only two studies have investigated whether the principles of the CI effect can be applied to the  
270 learning of upper-limb prosthesis skills – both of which utilised able-bodied users of prosthesis  
271 simulators. The first study, by Weeks et al.<sup>67</sup>, found that two days of random practice facilitated more  
272 proficient transfer of skills to novel tasks compared to blocked practice. This is important, as day-to-  
273 day prosthesis use will likely impose similar demands on an individual’s ability to transfer clinic-based  
274 training to unpredictable contexts and situations. In contrast, Bouwsema et al.<sup>68</sup> found that one day of  
275 either blocked or random practice resulted in similar performance levels during delayed retention and  
276 task-transfer tests. As the blocked practice facilitated greater performance during acquisition, the  
277 authors advocated a blocked schedule for prosthesis rehabilitation to achieve faster performance gains  
278 and thus optimise motivation. Such an interpretation should, however, be treated with caution given the  
279 small amount of practice (total 60 trials) included in the study.

280           These inconsistent results follow the observation that the typical CI effect is less robust when  
281 applied to non-laboratory skills<sup>69</sup>. To explain this, researchers have suggested that task complexity  
282 (relative to the performer) is likely to moderate the CI effect, and that task variability should be  
283 manipulated in a manner that brings about an “optimal challenge”<sup>70</sup>. However, as the challenge  
284 presented by a motor task will dynamically decrease with respect to an individual’s increasing skill  
285 proficiency, researchers have advocated for practice schedules that dynamically moderate CI (and thus  
286 challenge) across the practice session. For example, benefits have been shown for mixing blocked and  
287 random practice<sup>71</sup>, and systematically increasing CI across learning<sup>72</sup>. Benefits have also been shown  
288 for ‘learner adaptive’ practice schedules that regulate the frequency of task-switching based on trial-to-  
289 trial performance<sup>73,74</sup>. Typically, these adaptive schedules are designed to encourage increased task-  
290 switching when learners are performing well (increasing challenge) but decreased task-switching when  
291 learners are performing poorly (decreasing challenge), thus continually manipulating the appropriate  
292 levels of challenge. Research is needed to determine the utility of these adaptive schedules for prosthesis  
293 training and to determine the optimal success criteria for a task-switch (e.g., one versus two consecutive  
294 successes), which is a critical aspect of these schedules for moderating CI.

295           Taken together, the variability of a practice schedule is an aspect of rehabilitation design that  
296 should not be overlooked. A crucial point is that performance gains achieved during a practice (or  
297 therapy) session are not necessarily a good index of long-term motor adaptation. Consequently, both  
298 therapists and learners are potentially at risk of wrongly endorsing a highly repetitive (i.e., blocked)  
299 training strategy that seemingly facilitates more immediate performance, potentially to the detriment of  
300 long-term skill acquisition. Increasing the variability of practice through a random schedule could  
301 therefore be used to increase task difficulty, cognitive effort and the potential for learning and transfer.  
302 However, therapists should be mindful that a strictly random schedule might be too challenging for  
303 those learners struggling to control their prosthesis, leading to discouragement if the learner does not  
304 feel they are improving as well as might be expected<sup>75</sup>. This is problematic when considering that  
305 rehabilitation sessions are typically short in nature, thus minimising the time available to both the patient  
306 and therapist to observe meaningful practice benefits. Task variability could therefore be adaptively  
307 manipulated in a manner that brings about an optimal challenge for learners, maintaining moderate  
308 levels of performance error without disrupting motivation and the perceived usefulness of training.  
309 However, far greater research is needed to apply adaptive practice schedules to the context of prosthesis  
310 rehabilitation.

### 311           **3.5. Motor Imagery and Action Observation**

312           The implementation of mental simulation techniques could help facilitate the ability to use  
313 upper limb prosthetic devices. Action observation involves the observation of successful movement  
314 execution<sup>76</sup>, whilst motor imagery involves the intentional internal generation of visual and kinaesthetic  
315 aspects of movement<sup>77</sup>. Jeannerod's simulation theory<sup>78</sup> proposed that action observation and motor  
316 imagery are simulated forms of action, which elicit activity in similar brain regions to those involved  
317 in movement execution. Meta-analyses of neuroimaging data have confirmed that various brain regions  
318 active during movement execution are also active during both action observation and motor  
319 imagery<sup>79,80</sup>. Activation of motor-related brain regions through these processes is presumed to facilitate  
320 subsequent motor execution, with the repeated activation in this manner assumed to promote Hebbian  
321 plasticity in a similar manner to physical practice<sup>81</sup>. The efficacy of these techniques has been explored

322 in various movement rehabilitation contexts. Both techniques, when implemented alongside physical  
323 therapy, can promote improvements in motor function in individuals with motor impairments associated  
324 with stroke<sup>82</sup>, Parkinson's Disease<sup>83</sup>, and Developmental Coordination Disorder<sup>84</sup>.

325         Given the positive effects reported for action observation and motor imagery in movement  
326 rehabilitation contexts, it is noteworthy that these techniques have received relatively little research  
327 attention in relation to upper-limb prosthesis training. However, several researchers have explored the  
328 efficacy of action observation training on the acquisition of prosthetic hand control. For example,  
329 Cusack et al.<sup>85</sup> showed that those who trained to use a prosthesis by observing and imitating the  
330 movements of prosthesis users were able to execute actions with reduced movement variability,  
331 compared to those who trained by observing and imitating the movements of intact limbs. Bayani et  
332 al.<sup>86</sup> reported similar findings, with greater kinematic improvements following training involving action  
333 observation of a prosthesis user compared to action observation of an intact limb. Eye-tracking  
334 measures also revealed that different gaze strategies underpinned the kinematic differences, with those  
335 observing intact limbs directing their gaze primarily to the start and end points of the observed action,  
336 and those observing prosthesis use directing their gaze towards the path of the prosthesis in action and  
337 the shoulders.

338         There have been some attempts to develop upper-limb prosthetic devices that can be controlled  
339 by motor imagery through a brain-computer interface<sup>87</sup>. However, we are not aware of any research that  
340 has investigated the efficacy of motor imagery techniques to aid the learning of a prosthetic device.  
341 This is surprising in relation to myoelectric prosthetic devices, as the use of kinaesthetic imagery to  
342 mentally rehearse the generation of the signals required to activate the device could conceivably aid  
343 users in learning the control mechanisms of the device.

344         In the past decade, there has been an increased focus on the combined and simultaneous use of  
345 action observation and motor imagery (i.e., AOMI). This approach involves instructing individuals to  
346 observe an action on video, whilst engaging simultaneously in kinaesthetic imagery of the sensations  
347 associated executing the observed movement. Neurophysiological research has shown that this  
348 approach elicits increased activity in the motor system than either independent action observation or

349 independent motor imagery<sup>88</sup>. There is also evidence that this combined approach is effective in  
350 facilitating motor performance. For example, Marshall et al.<sup>89</sup> showed that AOMI improves eye-hand  
351 coordination and performance in a novel visuomotor task to a greater extent than action observation  
352 alone. AOMI could therefore prove to be effective for the learning of myoelectric prosthetic devices, as  
353 the action observation component would convey important kinematic information, such as the optimal  
354 limb orientation and positioning required to interact successfully with objects, whilst the motor imagery  
355 component could facilitate the learning of the control mechanisms associated with generating  
356 myosignals to activate the device.

357         Exploration of the effects of motor simulation techniques on learning to use a prosthetic hand  
358 would be a worthwhile line of future investigation. If found to be effective, these strategies could have  
359 considerable implications for prosthesis training. For example, as these techniques do not require overt  
360 action it would be possible for individuals to begin the process of learning to use a prosthesis at an  
361 earlier point, prior to planned amputations, as well as during the pre-prosthetic phase post-amputation  
362 when movement is impaired. This could enhance the rate at which individuals become skilled in using  
363 their prosthesis, potentially enhancing prosthesis adoption rates. Training through action observation  
364 and motor imagery techniques could also alleviate fatigue and soreness associated with repetitive  
365 physical training with the prosthesis in the initial days and weeks post-amputation. These methods could  
366 also offer a convenient and cost-effective therapy to be prescribed by occupational therapists, which  
367 can be employed at the user's convenience, either alongside regular training or in isolation.

### 368         **3.6. Virtual Training and Biofeedback**

369         Virtual training and biofeedback are becoming increasingly important aspects in the upper-limb  
370 prosthesis rehabilitation process. These methods are advantageous, as they do not require a fully healed  
371 stump, meaning they can be implemented far before the initiation of conventional prosthesis training.  
372 This is especially important considering that starting training early has been shown to result in higher  
373 acceptance and use of the prosthesis<sup>90</sup>. The main premise of virtual training and biofeedback in upper-  
374 limb rehabilitation is to enhance someone's myocontrol, which is the ability to control the opening and  
375 closing of a myoelectric prosthesis through surface EMG signals derived from the action potentials

376 produced by (usually two) muscles<sup>91</sup>. Good myocontrol is a prerequisite of functional prosthesis use,  
377 especially considering the increasing dexterity of the latest myoelectric devices. Indeed, experienced  
378 users of a myoelectric prosthesis have been shown to generate more consistent prosthesis control  
379 following EMG biofeedback<sup>92</sup>. However, the ability to produce distinct myosignals is not intuitive and  
380 can vary on an individual basis<sup>93</sup>. Therefore, virtual training and biofeedback provide potentially  
381 promising techniques to develop myocontrol in the pre-prosthetic stage.

382         Three main methods for training the myosignal have been examined by research. The first  
383 simply involves displaying a live feed of EMG signals on a computer screen, representative of basic  
384 biofeedback. The second and third are more representative of virtual training and involve either  
385 displaying a virtual prosthesis on a screen that is manipulated via the myosignal in the exact manner as  
386 an actual prosthesis<sup>94</sup>, or incorporating control of the myosignal into controlling an aspect of a computer  
387 game<sup>95</sup>. These methods have shown positive results for enhancing control of the myosignal in upper-  
388 limb prostheses. For example, Bouwsema et al.<sup>93</sup> found training with a virtual hand to be equivalent to  
389 training with a physical prosthesis, advocating virtual training as a vital component of prosthesis  
390 training to enhance motivation and expedite learning during the early stages of skill development.  
391 Nakamura et al.<sup>96</sup> demonstrated that training with virtual myocontrol software transferred to a grasping  
392 task performed with a physical prosthesis, namely a box and block test, with improvements in both the  
393 number of blocks moved and the orientation of the hand on approach. There is also some evidence that  
394 the benefits of virtual training may extend beyond convenience and efficiency. For example, in a study  
395 using virtual avatars and EEG, Fernandez-Vargas et al.<sup>97</sup> found that imitating movements presented  
396 virtually resulted in greater parietal alpha desynchronisation during motion, which may be suggestive  
397 of lower attentional demands for the trainee. Most of the studies advocating the use of virtual training  
398 to date have been performed with healthy participants but in a recent study with upper-extremity  
399 amputees, Perry et al.<sup>98</sup> found that training with a virtual avatar controlled by the myosignal improved  
400 movement accuracy across three different motion sets of varied complexity.

401         Although these methods have been shown to have comparable learning advantages for  
402 prosthesis training<sup>91</sup>, various authors have suggested that a computer game would be most beneficial as



403 it has the potential to be more engaging and fun than the other methods<sup>91</sup>. For example, Radhakrishnan  
404 et al.<sup>99</sup> developed a game-based pre-prosthesis training environment designed to challenge users to  
405 reach higher scores. Using an evaluation questionnaire, they found that participants responded  
406 positively to the games, reporting enjoyment regarding the varied levels of difficulty and motivation to  
407 return to the game. Participants also reported that they believed the games could be used to improve  
408 their muscular control. However, this study was performed with healthy participants and further  
409 investigation with limb-loss patients is warranted.

410         These virtual systems benefit from being low cost, portable, and easy to use, allowing users to  
411 practice at home without a therapist and have autonomy over practice type and difficulty. Additionally,  
412 the level of myocontrol displayed during pre-prosthetic training can also be used to determine the  
413 suitability of potential prosthesis control components, making for a more personalised device. However,  
414 the field needs an easily administrable test to identify myocontrol learning ability and standardise this  
415 protocol<sup>91</sup>. Another important point for consideration is the distinct difference between operating a  
416 virtual and physical prosthesis. Training with a physical prosthesis poses postural kinetic and kinematic  
417 challenges that are not addressed by virtual training. This may limit the application of virtual training  
418 to myoelectric control primarily. Furthermore, if virtual training is to be applied into a prosthesis  
419 training protocols, more information is needed about how it would be implemented and whether it could  
420 be integrated with the motor learning principles discussed in the present review. Research into this area  
421 could significantly enhance the already promising learning benefits of virtual training and biofeedback,  
422 optimizing the time an amputee spends in the pre-prosthetic stage.

#### 423         **4. Conclusion**

424         Current rates of upper-limb prosthesis abandonment remain high, with technological  
425 advancements yet to achieve any significant impact on user satisfaction<sup>1</sup>. The importance of optimising  
426 early and appropriate training therefore cannot be overlooked. While the intuition and experience of  
427 clinicians holds enormous value, evidence-based guidelines based on well-established motor learning  
428 principles will also be crucial for training effective prosthetic hand control. Important to the design of  
429 any such guidelines is the realisation that the level of limb-loss and the type of device are important

430 factors in need of consideration. For example, patients with more proximal levels of limb-loss have  
431 difficulties with bimanual tasks<sup>100</sup>, higher abandonment rates <sup>101</sup>, report less satisfaction<sup>102</sup>, and lower  
432 perceived functionality<sup>103</sup> compared to users of below elbow prostheses. There is also evidence that  
433 prosthetic devices with pattern-recognition technology can optimise intuitive control and alleviate  
434 cognitive demands compared to more traditional devices using direct control schemes<sup>104,105</sup>. We  
435 therefore are not proposing the pursuit of a ‘gold-standard’ one size fits all approach to training, instead  
436 we are advocating for an evidence-based approach that provides applied practitioners with a ‘tool-box’  
437 of research-informed techniques that can be used in a client-centred manner based on their experiential  
438 knowledge. It is clear that more research is needed before this is achieved and it is hoped that this review  
439 highlights the potential avenues for such work. Finally, a challenge moving forward is ensuring that  
440 any growth in academic knowledge achieves some degree of clinical translation. Future attempts to  
441 optimise prosthesis training should therefore attempt to engage in multi-stakeholder collaborations  
442 between users, researchers, clinicians, charity representatives and industry specialists to achieve greater  
443 impact and benefit for the target population<sup>106</sup>.

444

- 445 1. Salminger S, Stino H, Pichler LH, et al. Current rates of prosthetic usage in upper-limb  
446 amputees – have innovations had an impact on device acceptance? *Disabil Rehabil.*  
447 2020;0(0):1-12. doi:10.1080/09638288.2020.1866684
- 448 2. Yamamoto M, Chung KC, Sterbenz J, et al. Cross-sectional International Multicenter Study on  
449 Quality of Life and Reasons for Abandonment of Upper Limb Prostheses. *Plast Reconstr Surg*  
450 *Glob Open.* 2019;7(5):e2205. doi:10.1097/GOX.0000000000002205
- 451 3. Resnik L, Borgia M, Biester S, Clark MA. Longitudinal study of prosthesis use in veterans with  
452 upper limb amputation. *Prosthet Orthot Int.* Published online October 6,  
453 2020:0309364620957920. doi:10.1177/0309364620957920
- 454 4. Gambrell CR. Overuse Syndrome and the Unilateral Upper Limb Amputee: Consequences and  
455 Prevention. *JPO J Prosthet Orthot.* 2008;20(3):126-132. doi:10.1097/JPO.0b013e31817ecb16
- 456 5. Biddiss EA, Chau TT. Upper limb prosthesis use and abandonment: A survey of the last 25  
457 years. *Prosthet Orthot Int.* 2007;31(3):236-257. doi:10.1080/03093640600994581
- 458 6. Smail LC, Neal C, Wilkins C, Packham TL. Comfort and function remain key factors in upper  
459 limb prosthetic abandonment: findings of a scoping review. *Disabil Rehabil Assist Technol.*  
460 2020;0(0):1-10. doi:10.1080/17483107.2020.1738567
- 461 7. Engdahl SM, Christie BP, Kelly B, Davis A, Chestek CA, Gates DH. Surveying the interest of  
462 individuals with upper limb loss in novel prosthetic control techniques. *J NeuroEngineering*  
463 *Rehabil.* 2015;12(1):53. doi:10.1186/s12984-015-0044-2
- 464 8. Antfolk C, D'Alonzo M, Rosén B, Lundborg G, Sebelius F, Cipriani C. Sensory feedback in upper  
465 limb prosthetics. *Expert Rev Med Devices.* 2013;10(1):45-54. doi:10.1586/erd.12.68
- 466 9. Parajuli N, Sreenivasan N, Bifulco P, et al. Real-Time EMG Based Pattern Recognition Control  
467 for Hand Prostheses: A Review on Existing Methods, Challenges and Future Implementation.  
468 *Sensors.* 2019;19(20):4596. doi:10.3390/s19204596
- 469 10. Atkins DJ, Sturma A. Principles of Occupational and Physical Therapy in Upper Limb  
470 Amputations. In: Aszmann OC, Farina D, eds. *Bionic Limb Reconstruction.* Springer  
471 International Publishing; 2021:197-214. doi:10.1007/978-3-030-60746-3\_20
- 472 11. Brenner CD, Brenner JK. The Use of Preparatory/Evaluation/Training Prostheses in Developing  
473 Evidenced-Based Practice in Upper Limb Prosthetics. *JPO J Prosthet Orthot.* 2008;20(3):70-82.  
474 doi:10.1097/JPO.0b013e31817c59fb
- 475 12. Lake C, Dodson R. Progressive upper limb prosthetics. *Phys Med Rehabil Clin N Am.*  
476 2006;17(1):49-72. doi:10.1016/j.pmr.2005.10.004
- 477 13. Østlie K, Skjeldal OH, Garfelt B, Magnus P. Adult acquired major upper limb amputation in  
478 Norway: prevalence, demographic features and amputation specific features. A population-  
479 based survey. *Disabil Rehabil.* 2011;33(17-18):1636-1649.  
480 doi:10.3109/09638288.2010.541973
- 481 14. Ramstrand N, Brodtkorb T-H. Considerations for developing an evidenced-based practice in  
482 orthotics and prosthetics. *Prosthet Orthot Int.* 2008;32(1):93-102.  
483 doi:10.1080/03093640701838190

- 484 15. Bouwsema H, van der Sluis CK, Bongers RM. Changes in performance over time while learning  
485 to use a myoelectric prosthesis. *J NeuroEngineering Rehabil.* 2014;11(1):16.  
486 doi:10.1186/1743-0003-11-16
- 487 16. Bouwsema H, Kyberd PJ, Hill W, van der Sluis CK, Bongers RM. Determining skill level in  
488 myoelectric prosthesis use with multiple outcome measures. *J Rehabil Res Dev.*  
489 2012;49(9):1331-1348. doi:10.1682/jrrd.2011.09.0179
- 490 17. Kal E, Houdijk H, Van Der Wurff P, et al. The inclination for conscious motor control after  
491 stroke: validating the Movement-Specific Reinvestment Scale for use in inpatient stroke  
492 patients. *Disabil Rehabil.* 2016;38(11):1097-1106. doi:10.3109/09638288.2015.1091858
- 493 18. Masters RSW, Pall HS, MacMahon KMA, Eves FF. Duration of Parkinson Disease Is Associated  
494 With an Increased Propensity for "Reinvestment." *Neurorehabil Neural Repair.*  
495 2007;21(2):123-126. doi:10.1177/1545968306290728
- 496 19. Parr JVV, Vine SJ, Wilson MR, Harrison NR, Wood G. Visual attention, EEG alpha power and  
497 T7-Fz connectivity are implicated in prosthetic hand control and can be optimized through  
498 gaze training. *J NeuroEngineering Rehabil.* 2019;16(1):52. doi:10.1186/s12984-019-0524-x
- 499 20. Wulf G. Attentional focus and motor learning: a review of 15 years. *Int Rev Sport Exerc*  
500 *Psychol.* 2013;6(1):77-104. doi:10.1080/1750984X.2012.723728
- 501 21. Wulf G, Prinz W. Directing attention to movement effects enhances learning: A review.  
502 *Psychon Bull Rev.* 2001;8(4):648-660. doi:10.3758/BF03196201
- 503 22. Bell JJ, Hardy J. Effects of Attentional Focus on Skilled Performance in Golf. *J Appl Sport*  
504 *Psychol.* 2009;21(2):163-177. doi:10.1080/10413200902795323
- 505 23. Kim T, Díaz JJ, Chen J. The effect of attentional focus in balancing tasks: A systematic review  
506 with meta-analysis. *J Hum Sport Exerc.* 2017;12(2):463-479.
- 507 24. Wulf G, Dufek JS. Increased Jump Height with an External Focus Due to Enhanced Lower  
508 Extremity Joint Kinetics. *J Mot Behav.* 2009;41(5):401-409. doi:10.1080/00222890903228421
- 509 25. Marchant DC, Greig M, Scott C. Attentional Focusing Instructions Influence Force Production  
510 and Muscular Activity During Isokinetic Elbow Flexions. *J Strength Cond Res.* 2009;23(8):2358-  
511 2366. doi:10.1519/JSC.0b013e3181b8d1e5
- 512 26. Kristoffersen MB, Franzke AW, van der Sluis CK, Murgia A, Bongers RM. Serious gaming to  
513 generate separated and consistent EMG patterns in pattern-recognition prosthesis control.  
514 *Biomed Signal Process Control.* 2020;62:102140. doi:10.1016/j.bspc.2020.102140
- 515 27. Kristoffersen MB, Franzke AW, Bongers RM, Wand M, Murgia A, van der Sluis CK. User  
516 training for machine learning controlled upper limb prostheses: a serious game approach. *J*  
517 *NeuroEngineering Rehabil.* 2021;18(1):32. doi:10.1186/s12984-021-00831-5
- 518 28. Mak TCT, Young WR, Chan DCL, Wong TWL. Gait Stability in Older Adults During Level-Ground  
519 Walking: The Attentional Focus Approach. *J Gerontol Ser B.* 2020;75(2):274-281.  
520 doi:10.1093/geronb/gby115

- 521 29. Lohse KR, Sherwood DE. Thinking about muscles: The neuromuscular effects of attentional  
522 focus on accuracy and fatigue. *Acta Psychol (Amst)*. 2012;140(3):236-245.  
523 doi:10.1016/j.actpsy.2012.05.009
- 524 30. Lohse KR, Sherwood DE, Healy AF. Neuromuscular Effects of Shifting the Focus of Attention in  
525 a Simple Force Production Task. *J Mot Behav*. 2011;43(2):173-184.  
526 doi:10.1080/00222895.2011.555436
- 527 31. Kuhn Y-A, Keller M, Ruffieux J, Taube W. Adopting an external focus of attention alters  
528 intracortical inhibition within the primary motor cortex. *Acta Physiol*. 2017;220(2):289-299.  
529 doi:10.1111/apha.12807
- 530 32. Kuhn Y-A, Keller M, Ruffieux J, Taube W. Intracortical Inhibition Within the Primary Motor  
531 Cortex Can Be Modulated by Changing the Focus of Attention. *JoVE J Vis Exp*.  
532 2017;(127):e55771. doi:10.3791/55771
- 533 33. Masters RSW, Duijn T van, Uiga L. Advances in implicit motor learning. In: *Skill Acquisition in*  
534 *Sport*. 3rd ed. Routledge; 2019.
- 535 34. Masters RSW. Knowledge, knerves and know-how: The role of explicit versus implicit  
536 knowledge in the breakdown of a complex motor skill under pressure. *Br J Psychol*.  
537 1992;83(3):343-358. doi:10.1111/j.2044-8295.1992.tb02446.x
- 538 35. Masters R, Maxwell J. The theory of reinvestment. *Int Rev Sport Exerc Psychol*. 2008;1(2):160-  
539 183. doi:10.1080/17509840802287218
- 540 36. Capio CM, Sit CHP, Abernethy B, Masters RSW. Fundamental movement skills and physical  
541 activity among children with and without cerebral palsy. *Res Dev Disabil*. 2012;33(4):1235-  
542 1241. doi:10.1016/j.ridd.2012.02.020
- 543 37. Maxwell JP, Masters RSW, Kerr E, Weedon E. The implicit benefit of learning without errors. *Q*  
544 *J Exp Psychol Sect A*. 2001;54(4):1049-1068. doi:10.1080/713756014
- 545 38. Poolton JM, Masters RSW, Maxwell JP. Passing thoughts on the evolutionary stability of  
546 implicit motor behaviour: Performance retention under physiological fatigue. *Conscious Cogn*.  
547 2007;16(2):456-468. doi:10.1016/j.concog.2006.06.008
- 548 39. Capio CM, Poolton JM, Sit CHP, Eguia KF, Masters RSW. Reduction of errors during practice  
549 facilitates fundamental movement skill learning in children with intellectual disabilities. *J*  
550 *Intellect Disabil Res*. 2013;57(4):295-305. doi:10.1111/j.1365-2788.2012.01535.x
- 551 40. van der Kamp J, Steenbergen B, Masters RSW. Explicit and implicit motor learning in children  
552 with unilateral cerebral palsy. *Disabil Rehabil*. 2018;40(23):2790-2797.  
553 doi:10.1080/09638288.2017.1360403
- 554 41. Masters RSW, MacMahon KMA, Pall HS. Implicit Motor Learning in Parkinson's Disease.  
555 *Rehabil Psychol*. 2004;49(1):79-82. doi:10.1037/0090-5550.49.1.79
- 556 42. Orrell AJ, Eves FF, Masters RS. Motor Learning of a Dynamic Balancing Task After Stroke:  
557 Implicit Implications for Stroke Rehabilitation. *Phys Ther*. 2006;86(3):369-380.  
558 doi:10.1093/ptj/86.3.369

- 559 43. Chauvel G, Maquestiaux F, Gemonet E, et al. Intact Procedural Knowledge in Patients with  
560 Alzheimer's Disease: Evidence from Golf Putting. *J Mot Behav.* 2018;50(3):268-274.  
561 doi:10.1080/00222895.2017.1341376
- 562 44. van Abswoude F, Santos-Vieira B, van der Kamp J, Steenbergen B. The influence of errors  
563 during practice on motor learning in young individuals with cerebral palsy. *Res Dev Disabil.*  
564 2015;45-46:353-364. doi:10.1016/j.ridd.2015.08.008
- 565 45. Donaghey C, McMillan T, O'Neill B. Errorless learning is superior to trial and error when  
566 learning a practical skill in rehabilitation: a randomized controlled trial. *Clin Rehabil.*  
567 2010;24(3):195-201. doi:10.1177/0269215509353270
- 568 46. Liao C-M, Masters RSW. Analogy learning: A means to implicit motor learning. *J Sports Sci.*  
569 2001;19(5):307-319. doi:10.1080/02640410152006081
- 570 47. Koedijker JM, Poolton JM, Maxwell JP, Oudejans RRD, Beek PJ, Masters RSW. Attention and  
571 time constraints in perceptual-motor learning and performance: Instruction, analogy, and skill  
572 level. *Conscious Cogn.* 2011;20(2):245-256. doi:10.1016/j.concog.2010.08.002
- 573 48. Lam WK, Maxwell JP, Masters R. Analogy Learning and the Performance of Motor Skills under  
574 Pressure. *J Sport Exerc Psychol.* 2009;31(3):337-357. doi:10.1123/jsep.31.3.337
- 575 49. Schlapkohl N, Hohmann T, Raab M. Effects of instructions on performance outcome and  
576 movement patterns for novices and experts in table tennis. *Int J Sport Psychol.*  
577 2012;43(6):522-541.
- 578 50. Kleynen M, Jie L-J, Theunissen K, et al. The immediate influence of implicit motor learning  
579 strategies on spatiotemporal gait parameters in stroke patients: a randomized within-subjects  
580 design. *Clin Rehabil.* 2019;33(4):619-630. doi:10.1177/0269215518816359
- 581 51. Jie L-J, Goodwin V, Kleynen M, Braun S, Nunns M, Wilson M. Analogy learning in Parkinson's  
582 disease: A proof-of-concept study. *Int J Ther Rehabil.* 2016;23(3):123-130.  
583 doi:10.12968/ijtr.2016.23.3.123
- 584 52. Parr JVV, Vine SJ, Harrison NR, Wood G. Examining the Spatiotemporal Disruption to Gaze  
585 When Using a Myoelectric Prosthetic Hand. *J Mot Behav.* 2018;50(4):416-425.  
586 doi:10.1080/00222895.2017.1363703
- 587 53. Chadwell A, Kenney L, Granat MH, et al. Upper limb activity in myoelectric prosthesis users is  
588 biased towards the intact limb and appears unrelated to goal-directed task performance. *Sci*  
589 *Rep.* 2018;8(1):11084. doi:10.1038/s41598-018-29503-6
- 590 54. Land MF. Vision, eye movements, and natural behavior. *Vis Neurosci.* 2009;26(1):51-62.  
591 doi:10.1017/S0952523808080899
- 592 55. Sailer U, Flanagan JR, Johansson RS. Eye-Hand Coordination during Learning of a Novel  
593 Visuomotor Task. *J Neurosci.* 2005;25(39):8833-8842. doi:10.1523/JNEUROSCI.2658-05.2005
- 594 56. Vine SJ, Masters RSW, McGrath JS, Bright E, Wilson MR. Cheating experience: Guiding novices  
595 to adopt the gaze strategies of experts expedites the learning of technical laparoscopic skills.  
596 *Surgery.* 2012;152(1):32-40. doi:10.1016/j.surg.2012.02.002

- 597 57. Bosch TJ, Hanna T, Fercho KA, Baugh LA. Behavioral performance and visual strategies during  
598 skill acquisition using a novel tool use motor learning task. *Sci Rep.* 2018;8(1):13755.  
599 doi:10.1038/s41598-018-32001-4
- 600 58. Chadwell A, Kenney L, Thies S, Galpin A, Head J. The Reality of Myoelectric Prostheses:  
601 Understanding What Makes These Devices Difficult for Some Users to Control. *Front*  
602 *Neurorobotics.* 2016;0. doi:10.3389/fnbot.2016.00007
- 603 59. Chadwell A, Kenney L, Thies S, Head J, Galpin A, Baker R. Addressing unpredictability may be  
604 the key to improving performance with current clinically prescribed myoelectric prostheses.  
605 *Sci Rep.* 2021;11(1):3300. doi:10.1038/s41598-021-82764-6
- 606 60. Wilson MR, Vine SJ, Bright E, Masters RSW, Defriend D, McGrath JS. Gaze training enhances  
607 laparoscopic technical skill acquisition and multi-tasking performance: a randomized,  
608 controlled study. *Surg Endosc.* 2011;25(12):3731-3739. doi:10.1007/s00464-011-1802-2
- 609 61. Parr JVV, Gallicchio G, Wood G. EEG correlates of verbal and conscious processing of motor  
610 control in sport and human movement: a systematic review. *Int Rev Sport Exerc Psychol.*  
611 2021;0(0):1-32. doi:10.1080/1750984X.2021.1878548
- 612 62. Shea JB, Morgan RL. Contextual interference effects on the acquisition, retention, and  
613 transfer of a motor skill. *J Exp Psychol [Hum Learn].* 1979;5(2):179-187. doi:10.1037/0278-  
614 7393.5.2.179
- 615 63. Lee TD, Simon DA. Contextual interference. In: *Skill Acquisition in Sport.* Routledge; 2004.
- 616 64. Broadbent DP, Causer J, Ford PR, Williams AM. Contextual interference effect on perceptual-  
617 cognitive skills training. *Med Sci Sports Exerc.* 2015;47(6):1243-1250.  
618 doi:10.1249/MSS.0000000000000530
- 619 65. Cross ES, Schmitt PJ, Grafton ST. Neural Substrates of Contextual Interference during Motor  
620 Learning Support a Model of Active Preparation. *J Cogn Neurosci.* 2007;19(11):1854-1871.  
621 doi:10.1162/jocn.2007.19.11.1854
- 622 66. Lin C-H (Janice), Winstein CJ, Fisher BE, Wu AD. Neural Correlates of the Contextual  
623 Interference Effect in Motor Learning: A Transcranial Magnetic Stimulation Investigation. *J*  
624 *Mot Behav.* 2010;42(4):223-232. doi:10.1080/00222895.2010.492720
- 625 67. Weeks DL, Anderson DI, Wallace SA. The Role of Variability in Practice Structure when  
626 Learning to Use an Upper-Extremity Prosthesis. *JPO J Prosthet Orthot.* 2003;15(3):84-92.
- 627 68. Bouwsema H, van der Sluis CK, Bongers RM. The Role of Order of Practice in Learning to  
628 Handle an Upper-Limb Prosthesis. *Arch Phys Med Rehabil.* 2008;89(9):1759-1764.  
629 doi:10.1016/j.apmr.2007.12.046
- 630 69. Barreiros J, Figueiredo T, Godinho M. The contextual interference effect in applied settings.  
631 *Eur Phys Educ Rev.* 2007;13(2):195-208. doi:10.1177/1356336X07076876
- 632 70. Guadagnoli MA, Lee TD. Challenge Point: A Framework for Conceptualizing the Effects of  
633 Various Practice Conditions in Motor Learning. *J Mot Behav.* 2004;36(2):212-224.  
634 doi:10.3200/JMBR.36.2.212-224

- 635 71. Landin D, Hebert EP. A comparison of three practice schedules along the contextual  
636 interference continuum. *Res Q Exerc Sport*. 1997;68(4):357-361.  
637 doi:10.1080/02701367.1997.10608017
- 638 72. Porter JM, Magill RA. Systematically increasing contextual interference is beneficial for  
639 learning sport skills. *J Sports Sci*. 2010;28(12):1277-1285. doi:10.1080/02640414.2010.502946
- 640 73. Simon DA, Lee TD, Cullen JD. Win-Shift, Lose-Stay: Contingent Switching and Contextual  
641 Interference in Motor Learning. *Percept Mot Skills*. 2008;107(2):407-418.  
642 doi:10.2466/pms.107.2.407-418
- 643 74. Porter C, Greenwood D, Panchuk D, Pepping G-J. Learner-adapted practice promotes skill  
644 transfer in unskilled adults learning the basketball set shot. *Eur J Sport Sci*. 2020;20(1):61-71.  
645 doi:10.1080/17461391.2019.1611931
- 646 75. Simon DA, Bjork RA. Metacognition in motor learning. *J Exp Psychol Learn Mem Cogn*.  
647 2001;27(4):907-912. doi:10.1037/0278-7393.27.4.907
- 648 76. Neuman B, Gray R. A direct comparison of the effects of imagery and action observation on  
649 hitting performance. *Mov Sport Sci - Sci Mot*. 2013;(79):11-21. doi:10.1051/sm/2012034
- 650 77. Macintyre TE, Moran AP, Collet C, Guillot A. An emerging paradigm: a strength-based  
651 approach to exploring mental imagery. *Front Hum Neurosci*. 2013;0.  
652 doi:10.3389/fnhum.2013.00104
- 653 78. Jeannerod M. Neural Simulation of Action: A Unifying Mechanism for Motor Cognition.  
654 *NeuroImage*. 2001;14(1):S103-S109. doi:10.1006/nimg.2001.0832
- 655 79. Caspers S, Zilles K, Laird AR, Eickhoff SB. ALE meta-analysis of action observation and  
656 imitation in the human brain. *NeuroImage*. 2010;50(3):1148-1167.  
657 doi:10.1016/j.neuroimage.2009.12.112
- 658 80. Hardwick RM, Caspers S, Eickhoff SB, Swinnen SP. Neural correlates of action: Comparing  
659 meta-analyses of imagery, observation, and execution. *Neurosci Biobehav Rev*. 2018;94:31-  
660 44. doi:10.1016/j.neubiorev.2018.08.003
- 661 81. Holmes P, Calmels C. A Neuroscientific Review of Imagery and Observation Use in Sport. *J Mot  
662 Behav*. 2008;40(5):433-445. doi:10.3200/JMBR.40.5.433-445
- 663 82. Ertelt D, Small S, Solodkin A, et al. Action observation has a positive impact on rehabilitation  
664 of motor deficits after stroke. *NeuroImage*. 2007;36:T164-T173.  
665 doi:10.1016/j.neuroimage.2007.03.043
- 666 83. Buccino G. Action observation treatment: a novel tool in neurorehabilitation. *Philos Trans R  
667 Soc B Biol Sci*. 2014;369(1644):20130185. doi:10.1098/rstb.2013.0185
- 668 84. Marshall B, Wright DJ, Holmes PS, Williams J, Wood G. Combined action observation and  
669 motor imagery facilitates visuomotor adaptation in children with developmental coordination  
670 disorder. *Res Dev Disabil*. 2020;98:103570. doi:10.1016/j.ridd.2019.103570
- 671 85. Cusack WF, Patterson R, Thach S, Kistenberg RS, Wheaton LA. Motor performance benefits of  
672 matched limb imitation in prosthesis users. *Exp Brain Res*. 2014;232(7):2143-2154.  
673 doi:10.1007/s00221-014-3904-2



- 674 86. Bayani KY, Lawson RR, Levinson L, et al. Implicit development of gaze strategies support  
675 motor improvements during action encoding training of prosthesis use. *Neuropsychologia*.  
676 2019;127:75-83. doi:10.1016/j.neuropsychologia.2019.02.015
- 677 87. Elstob D, Secco EL. A Low Cost Eeg Based Bci Prosthetic Using Motor Imagery.  
678 *ArXiv160302869 Cs*. Published online March 9, 2016. Accessed August 5, 2021.  
679 <http://arxiv.org/abs/1603.02869>
- 680 88. Eaves DL, Riach M, Holmes PS, Wright DJ. Motor Imagery during Action Observation: A Brief  
681 Review of Evidence, Theory and Future Research Opportunities. *Front Neurosci*. 2016;0.  
682 doi:10.3389/fnins.2016.00514
- 683 89. Marshall B, Wright DJ, Holmes PS, Wood G. Combining Action Observation and Motor  
684 Imagery Improves Eye–Hand Coordination during Novel Visuomotor Task Performance. *J Mot*  
685 *Behav*. 2020;52(3):333-341. doi:10.1080/00222895.2019.1626337
- 686 90. Dakpa R, Heger H. Prosthetic management and training of adult upper limb amputees. *Curr*  
687 *Orthop*. 1997;11(3):193-202. doi:10.1016/S0268-0890(97)90034-7
- 688 91. Terlaak B, Bouwsema H, Sluis CK van der, Bongers RM. Virtual Training of the Myosignal. *PLOS*  
689 *ONE*. 2015;10(9):e0137161. doi:10.1371/journal.pone.0137161
- 690 92. Dosen S, Markovic M, Somer K, Graitmann B, Farina D. EMG Biofeedback for online predictive  
691 control of grasping force in a myoelectric prosthesis. *J NeuroEngineering Rehabil*.  
692 2015;12(1):55. doi:10.1186/s12984-015-0047-z
- 693 93. Bouwsema H, van der Sluis CK, Bongers RM. Learning to Control Opening and Closing a  
694 Myoelectric Hand. *Arch Phys Med Rehabil*. 2010;91(9):1442-1446.  
695 doi:10.1016/j.apmr.2010.06.025
- 696 94. Resnik L, Etter K, Klinger SL, Kambe C. Using virtual reality environment to facilitate training  
697 with advanced upper-limb prosthesis. *J Rehabil Res Dev*. 2011;48(6):707-718.  
698 doi:10.1682/jrrd.2010.07.0127
- 699 95. Davoodi R, Loeb GE. Development of a Physics-Based Target Shooting Game to Train  
700 Amputee Users of Multijoint Upper Limb Prostheses. *Presence Teleoperators Virtual Environ*.  
701 2012;21(1):85-95. doi:10.1162/PRES\_a\_00091
- 702 96. Nakamura G, Shibanoki T, Kurita Y, et al. A virtual myoelectric prosthesis training system  
703 capable of providing instructions on hand operations. *Int J Adv Robot Syst*.  
704 2017;14(5):1729881417728452. doi:10.1177/1729881417728452
- 705 97. Fernández-Vargas J, Tarvainen TVJ, Kita K, Yu W. Effects of Using Virtual Reality and Virtual  
706 Avatar on Hand Motion Reconstruction Accuracy and Brain Activity. *IEEE Access*.  
707 2017;5:23736-23750. doi:10.1109/ACCESS.2017.2766174
- 708 98. Perry BN, Armiger RS, Yu KE, et al. Virtual Integration Environment as an Advanced Prosthetic  
709 Limb Training Platform. *Front Neurol*. 2018;0. doi:10.3389/fneur.2018.00785
- 710 99. Radhakrishnan M, Smailagic A, French B, Siewiorek DP, Balan RK. Design and Assessment of  
711 Myoelectric Games for Prosthesis Training of Upper Limb Amputees. In: *2019 IEEE*  
712 *International Conference on Pervasive Computing and Communications Workshops (PerCom*  
713 *Workshops)*. ; 2019:151-157. doi:10.1109/PERCOMW.2019.8730824

- 714 100. Biddiss E, Beaton D, Chau T. Consumer design priorities for upper limb prosthetics. *Disabil*  
715 *Rehabil Assist Technol.* 2007;2(6):346-357. doi:10.1080/17483100701714733
- 716 101. McFarland LV, Hubbard Winkler SL, Heinemann AW, Jones M, Esquenazi A. Unilateral upper-  
717 limb loss: satisfaction and prosthetic-device use in veterans and servicemembers from  
718 Vietnam and OIF/OEF conflicts. *J Rehabil Res Dev.* 2010;47(4):299-316.  
719 doi:10.1682/jrrd.2009.03.0027
- 720 102. Resnik L, Borgia M, Heinemann AW, Clark MA. Prosthesis satisfaction in a national sample of  
721 Veterans with upper limb amputation. *Prosthet Orthot Int.* 2020;44(2):81-91.  
722 doi:10.1177/0309364619895201
- 723 103. Zhang X, Baun KS, Trent L, Miguelez JM, Kontson K. Factors influencing perceived function in  
724 the upper limb prosthesis user population. *PM&R.* 2021;n/a(n/a). doi:10.1002/pmrj.12697
- 725 104. White MM, Zhang W, Winslow AT, et al. Usability Comparison of Conventional Direct Control  
726 Versus Pattern Recognition Control of Transradial Prostheses. *IEEE Trans Hum-Mach Syst.*  
727 2017;47(6):1146-1157. doi:10.1109/THMS.2017.2759762
- 728 105. Deeny S, Chicoine C, Hargrove L, Parrish T, Jayaraman A. A Simple ERP Method for  
729 Quantitative Analysis of Cognitive Workload in Myoelectric Prosthesis Control and Human-  
730 Machine Interaction. *PLOS ONE.* 2014;9(11):e112091. doi:10.1371/journal.pone.0112091
- 731 106. Jones H, Dupan S, Coutinho M, et al. Co-Creation Facilitates Translational Research on Upper  
732 Limb Prosthetics. *Prosthesis.* 2021;3(2):110-118. doi:10.3390/prosthesis3020012
- 733