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# Corrigendum to “Biomechanical but not timed performance asymmetries persist between limbs 9 months after ACL reconstruction during planned and unplanned change of direction” [J. Biomech. 81 (2018) 93–103]

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The authors regret that the function used to normalise joint moments to body mass contained an error which resulted in incorrect calculation of these variables. Full re-analysis of the corrected data identified small differences from those originally reported in some effect sizes and phase boundaries for the relevant between-limb comparisons, but did not affect the conclusions of the study. Corrections to the text, tables and figures are detailed below, with changes to the corrected text highlighted in bold.

## Abstract

The abstract page states that ACLR side effect sizes were **0.72–0.50**. This should read 0.74–0.53.

## Results Section

### 3.2.1 Biomechanical differences between limbs:

The original text reads (errors highlighted in **bold**): The differences with the largest effect size was less internal knee valgus

moment on the ACLR limb in the middle of the stance phase (19–85%; ES 0.72). There was less knee flexion angle (19–84%; ES 0.57), ankle external rotation moment (19–83%; ES **0.56**), knee external rotation moment (19–82%; ES 0.54), knee extension moment (15–91%; ES **0.50**) as well as less knee internal rotation angle throughout all of stance phase (0–100%; ES 0.56) on the ACLR side.

**This should read:** The differences with the largest effect size was less internal knee valgus moment on the ACLR limb in the middle of the stance phase (19–85%; ES 0.74). There was less knee flexion angle (19–84%; ES 0.57), ankle external rotation moment (19–83%; ES; 0.57), knee external rotation moment (19–82%; ES 0.54), knee extension moment (15–91%; ES 0.53) as well as less knee internal rotation angle throughout all of stance phase (0–100%; ES 0.56) on the ACLR side.

The table below should replace Table 2.

Biomechanical differences between limbs (planned and unplanned combined)								
Variable	Direction	Start	End	ACLR (±STD)	95% CI	Non-ACLR (±STD)	95% CI	Effect size
Knee abduction moment (Nm/kg)	Valgus	19	85	0.45 (0.42)	0.40–0.50	0.97 (0.63)	0.89–1.05	0.74
Knee angle sagittal (°)	Flexion	19	84	55.3 (7.4)	54.4–56.2	60.3 (7.5)	59–61	0.57
Ankle moment transverse (Nm/kg)	External Rotation	19	83	−0.02 (0.16)	−0.04–0.00	0.16 (0.28)	0.13–0.20	0.57
Knee angle transverse (°)	Internal Rotation	0	100	16.2 (10.2)	14.9–17.4	22.6 (10.4)	21.2–23.8	0.56
Knee moment transverse (Nm/kg)	External Rotation	19	82	0.04 (0.14)	0.03–0.06	0.20 (0.27)	0.16–0.23	0.55
Knee moment sagittal (Nm/kg)	Extension	15	91	1.38 (0.51)	1.32–1.44	1.75 (0.48)	1.69–1.81	0.53

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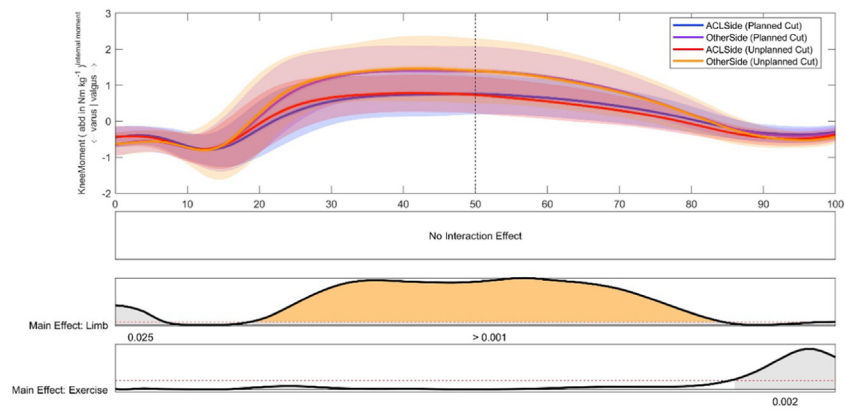
E-mail address: [endaking@hotmail.com](mailto:endaking@hotmail.com) (E. King).

<https://doi.org/10.1016/j.jbiomech.2020.110129>

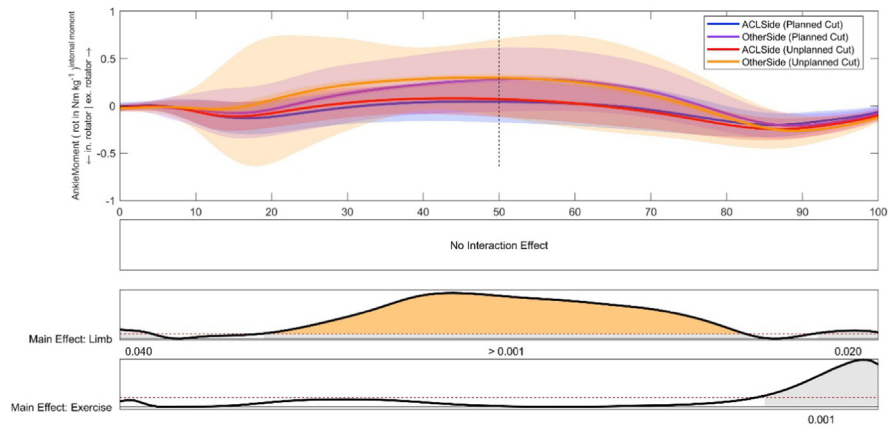
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The figures below, representing the joint moments, replace those in Appendix A (no changes to joint angles).

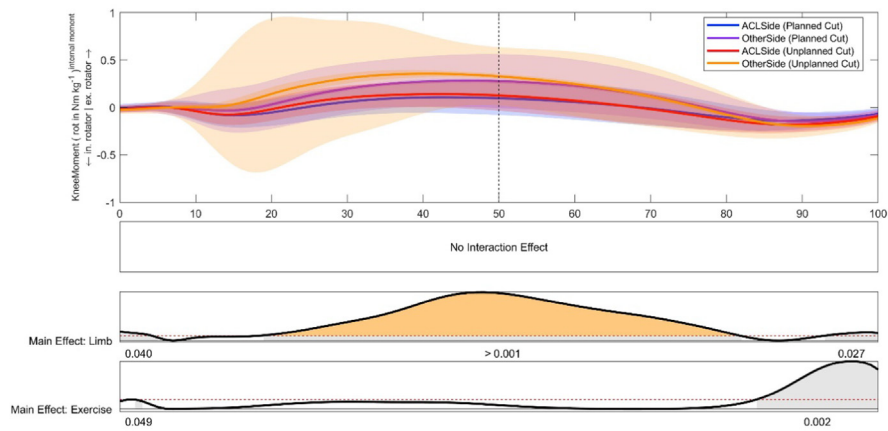
### Knee Moment Frontal



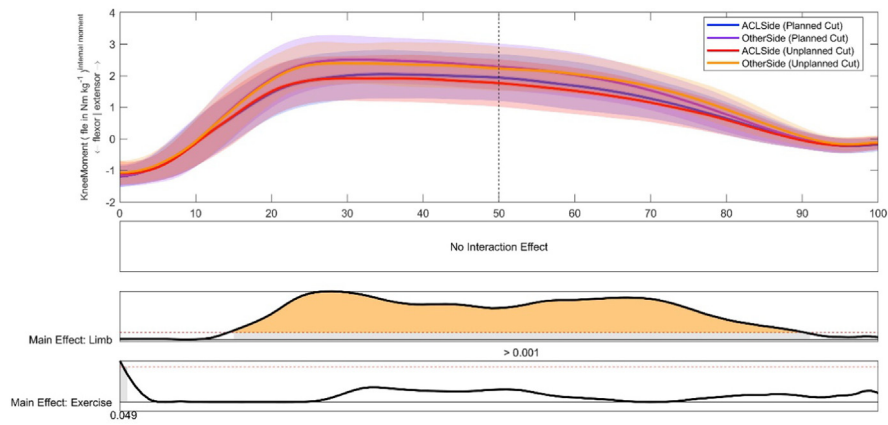
### Ankle Moment Transverse



### Knee Moment Transverse



## Knee Moment Sagittal



The authors would like to apologise for any inconvenience caused.