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ASSESSING MUSCLE STRENGTH ASYMMETRY VIA A UNILATERAL STANCE 1 **ISOMETRIC MID-THIGH PULL** 2 3

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51 Abstract

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Purpose: The purpose of this study was to investigate the within-session reliability of 53 bilateral and unilateral stance isometric mid-thigh pull (IMTP) force-time characteristics 54 including peak force (PF), relative PF and impulse at time bands (0-100, 0-200, 0-250 and 0-55 300 ms); and to compare isometric force-time characteristics between right and left and 56 57 dominant (D) and non-dominant (ND) limbs. Methods: Professional male Rugby league and multi-sport collegiate male athletes (n=54, age 23.4 ± 4.2 years, height 1.80 ± 0.05 m, mass: 58 88.9 ± 12.9 kg) performed 3 bilateral IMTP trials, and 3 unilateral stance IMTP trials per leg 59 60 on a force plate sampling at 600 Hz. Results: Intraclass correlation coefficients (ICC) and coefficients of variation (CV) demonstrated high-within session reliability for bilateral and 61 unilateral IMTP PF (ICC = .94, CV = 4.7-5.5%). Lower reliability measures and greater 62 63 variability were observed for bilateral and unilateral IMTP impulse at time bands (ICC =.81-.88, CV =7.7-11.8%). Paired sample t-tests and Cohen's d effect sizes revealed no significant 64 differences for all isometric force-time characteristics between right and left limbs in 65 collegiate male athletes (p >.05, $d \le 0.32$) and professional rugby league players (p >.05, d 66 67 ≤ 0.11), however significant differences were found between D and ND limbs in male collegiate athletes (p <.001, d = 0.43-0.91) and professional rugby league players (p < .001, d 68 = 0.27-0.46). Conclusion: This study demonstrated high within-session reliability for 69 70 unilateral stance IMTP PF; revealing significant differences in isometric force-time characteristics between D and ND limbs in male athletes. 71 72

73 *Keywords:* peak force, impulse, imbalance, reliability

75 Introduction

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Muscle strength asymmetry (MSA) refers to the relative strength differences and deficits 77 between limbs,¹ with a strength discrepancy of 10-15% or more between two sides 78 considered to represent a potentially problematic asymmetry.² Higher MSA indexes have been suggested to place athletes at a greater risk of injury,^{3 4, 5} conversely researchers have 79 80 demonstrated no connection between MSA and injury.^{6,7} However, there is no specific value 81 in the literature that represents the threshold between injured and non-injured athletes, or 82 values that definitively identify an increased injury risk in athletes.⁸ It should be noted that 83 asymmetries may be a positive adaptation of the sport, developed by specific sporting 84 demands.⁹ In terms of athletic performance previous studies have also shown MSA can 85 negatively impact performance during change of direction,¹⁰ vertical jumping,^{11, 12} and 86 kicking.¹³ However, asymmetry index values for athletic performance measures have yet to 87 be established.¹⁴ 88

89

Muscle strength asymmetry has typically been assessed in athletes via isokinetic 90 dynamometry,^{3, 14} vertical jump,¹² and multidirectional jump and hop tasks;¹⁵ with research 91 suggesting that the magnitude of MSA are task dependant.^{14, 15} More recently researchers 92 have investigated isometric bilateral asymmetries through isometric squat^{13, 16} and isometric 93 mid-thigh pull (IMTP)^{11, 17-19} assessments via a dual force plate system. Interestingly, 94 isometric asymmetrical differences have been observed between dominant (D) and non-95 dominant (ND) limbs for peak force,^{11, 17-19} and time-specific force values,^{18, 19} with 96 researchers reporting larger asymmetries in weaker athletes¹⁶⁻¹⁸ and female athletes^{18, 19} in 97 comparison to stronger athletes. Moreover, larger asymmetries have been associated with 98 lower jump heights and lower peak power in loaded and unloaded jumps.¹¹ However, block 99 periodised strength training has been shown to reduce bilateral asymmetries in weaker 100

athletes.¹⁶ Therefore, the assessment of lower limb MSA allows scientists and practitioners to
 monitor and identify higher imbalanced athletes to subsequently design effective training
 programs to reduce strength imbalances. This could potentially reduce risk of injury and
 improve athletic performance.

105

Jumping, sprinting and change of direction (COD) movements are unilateral, requiring 106 unilateral propulsive force production. Researchers have investigated unilateral force 107 production through unilateral jump assessments in relation to athletic performance tasks ^{10, 20} 108 and to investigate imbalances between lower limbs.^{15, 21} To our knowledge, previous 109 investigations have only assessed unilateral isometric force-time characteristics via an 110 unilateral isometric squat^{13, 22, 23} demonstrating high reliability measures. However, as IMTP 111 assessments are becoming more common in testing batteries in various athletic populations,^{18,} 112 ²⁴ and yield high reliability and low measurement error in force-time variables;^{24, 25} it is 113 somewhat surprising that a unilateral stance IMTP has yet to be investigated for assessing 114 115 MSA.

116

117 As previously stated bilateral asymmetries have been established during bilateral IMTP assessments via a dual force plate system, ^{11, 18, 19} however a unilateral stance IMTP would 118 allow direct comparisons between left and right limbs to establish any MSA indexes and the 119 identification of D and ND limbs. Furthermore, given the unilateral force production 120 requirements of sprinting, jumping and COD movements, arguably a unilateral stance IMTP 121 would be more specific to these dynamic sporting movements. Although the relationship of 122 MSA and injury risk remains inconclusive, from a performance perspective it would be 123 advantageous being equally proficient at producing force in both lower limbs,¹⁴ given the 124 unpredictable nature of multidirectional sports where athletes must change direction, jump 125 126 and land off either limb in response to stimuli.

127

The aims of this study were firstly to assess the within-session reliability of bilateral and 128 unilateral IMTP force-time characteristics (Peak force [PF], relative PF, impulse at time 129 bands 0-100, 0-200, 0-250, 0-300 ms). Secondly, to compare left and right and D and ND 130 limbs to determine if any significant differences and imbalances were present between limbs. 131 Thirdly, to establish normative MSA ranges for male collegiate athletes and professional 132 male rugby league players. It was hypothesized that the unilateral IMTP would demonstrate 133 high reliability, similar to the bilateral IMTP. Further, it was hypothesized that no significant 134 differences will be found in isometric force-time characteristic between left and right limbs, 135 136 but that significant differences would be observed between D and ND limbs.

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138 Methods

139

140 Subjects

54 male athletes consisting of 35 professional male rugby league players (age 24.2 ± 4.8 141 years, height 1.81 ± 0.06 m, mass 94.5 ± 11.2 kg) and 19 collegiate male athletes (soccer n=7, 142 rugby n=2, boxing n=2, weightlifting n=2, water polo n=1, cricket n=1, judo n=2, American 143 football n=2) (age 21.7 \pm 2.3 years, height 1.80 \pm 0.05 m, mass 78.4 \pm 7.9 kg) provided 144 informed consent to participate in this study which was approved by the institutional review 145 board. All subjects were familiar with the IMTP and possessed >2 years resistance training 146 experience. At the time of testing, the rugby athletes were at the end of pre-season and 147 148 collegiate athletes were currently in season.

- 149
- 150 Design

151 A within subjects design was used to determine any significant differences in isometric force-

time characteristics (PF, relative PF, impulse at time bands 0-100, 0-200, 0-250, 0-300 ms) between left and right and D and ND limbs during the unilateral IMTP; and to determine MSA indexes between limbs. Subjects performed three maximal bilateral IMTPs, and 3 unilateral stance IMTP trials per leg on a force plate sampling at 600 Hz. Within-session reliability was assessed for all isometric force-time characteristics for both bilateral and

- 157 unilateral IMTPs.
- 158

159 **Procedures**

160

161 **Pre-isometric warm up**

All subjects performed a standardized warm-up outlined in previous research,²⁶ comprising of 5 minutes of dynamic stretching before advancing to dynamic mid-thigh clean pulls. One set of 5 repetitions was performed with an empty barbell (Werksan Olympic Bar, Werksan, Moorsetown, NJ, USA) followed by 3 bilateral isometric efforts at perceived intensities of 50%, 70%, and 90% of maximum effort, interspersed with 1-minute recoveries.

167

168 Bilateral and unilateral isometric mid-thigh pull protocol

Bilateral IMTP testing followed similar protocols used in previous research.²⁷ The IMTP testing was performed on a portable force plate sampling at 600 Hz (400 Series Performance Force Plate, Fitness Technology, Adelaide, Australia) using a portable IMTP rack (Fitness Technology, Adelaide, Australia). Sampling as low as 500 Hz has been shown to produce high reliability measures for isometric force-time variables.²⁶ The force plate was interfaced with computer software [Ballistic Measurement System (BMS)] which allowed direct measurement of force-time characteristics.

For the bilateral stance IMTP testing, a collarless steel bar was positioned to correspond to 176 the athlete's second-pull power clean position²⁴ just below the crease of the hip. The bar 177 height could be adjusted (3 cm increments) at various heights above the force plate to 178 accommodate different sized athletes. Athletes were strapped to the bar in accordance to 179 previous research²⁸ and positioned in their self-selected mid-thigh clean position established 180 in the familiarization trials whereby feet were shoulder width apart, knees were flexed over 181 the toes, shoulders were just behind the bar, and torso was upright.²⁶ Researchers have 182 demonstrated that differences in knee and hip joint angles during the IMTP do not influence 183 kinetic variables²⁵ justifying the self-selected preferred mid-thigh position. All subjects 184 received standardized instructions to pull as fast and as hard as possible and push their feet 185 into the force plate until being told to stop, as these instructions have been shown to be 186 optimal in producing maximum PF and RFD results.²⁸ Once the body was stabilised (verified 187 by watching the subject and force trace) the IMTP was initiated with the countdown "3, 2, 1 188 pull," with subjects ensuring that maximal effort was applied for 5 seconds based on previous 189 protocols;^{24, 28} data was collected for a duration of 8 seconds. Minimal pre-tension was 190 allowed to ensure there is no slack in the body prior to initiation of pull. Verbal 191 encouragement was given for all trials and subjects. Subjects performed a total of 3 bilateral 192 maximal effort trials and interspersed with 2-minute recoveries. 193

194

195 Unilateral stance IMTP testing followed the same procedures outlined for bilateral IMTP 196 testing however was only performed with one foot on the force platform with the other limb 197 flexed 90° at the knee. Subjects were positioned at the same hip and knee joint angle 198 established during bilateral testing. Subjects were instructed to maintain balance and pull as 199 fast and as hard as possible and pushing their single foot into the force plate. Subjects performed a total of six unilateral maximum effort trials (3 with left and right limbs each) in
 an alternating order, interspersed with 2-minute recoveries. Any trials whereby subjects lost
 balance were excluded, and further trials were performed after a further 2-minute rest period.

203

204 Isometric Force-Time Curve Assessment

Isometric force-time data was analysed via BMS software. The maximum force recorded during the 5-second bilateral and unilateral IMTP trials was reported as PF. Relative PF was calculated PF / body mass. Impulse at 100 (IP 100), 200 (IP 200), 250 (IP 250) and 300 (IP 300) ms were also calculated (area under the force-time curve for each window) from onset of contraction (40 N threshold) and have demonstrated high reliability measures. ^{25, 27}

210 Statistical Analyses

- Statistical analysis was performed using SPSS software version 22 (SPSS, Chicago, Ill, USA)
 and a custom reliability spreadsheet.²⁹ Normality was confirmed for all variables using a
- and a custom reliability spreadsheet.²⁹ Normality was confirmed for all variables using a
 Shapiro Wilks-test. Within-session reliability was assessed via intraclass correlation
- coefficients (ICC), 95% confidence intervals (CI), coefficient of variation (CV), typical error
- of measurement (TE) expressed as CV between the three trials for each dependant variable
- using a custom spreadsheet²⁹ and percentage change in mean. The CV was calculated based
- on the mean square error term of logarithmically transformed data.²⁹ Minimum acceptable
- reliability was determined with an ICC > 0.7 and CV < 10%.^{30, 31} Mean ± SD were calculated for all dependent variables.
- 220

Asymmetry index (imbalance between right and left limbs) was calculated by the formulae 221 (right leg – left leg/ right leg \times 100) for unilateral IMTP variables.⁹ Asymmetry index for D 222 and ND limbs was calculated by the formulae (dominant leg - non dominant leg/ dominant 223 leg x 100) for unilateral IMTP variables, in accordance to previous research.⁹ Limb 224 dominance was defined as the limb that produced the highest isometric force-time value. To 225 assess the magnitude of differences in force-time characteristics between limbs in male 226 collegiate and professional rugby league players, paired sample t-tests and Cohen's d effect 227 sizes were implemented. Effect sizes were calculated by the formula Cohen's $d = M - M2/\sigma$ 228 pooled³² and interpreted as trivial (<0.19), small (0.20-0.59), moderate (0.60-1.19), large 229 (1.20–1.99), and very large (2.0-4.0).³³ The criterion for significance was set at p < 0.05. 230

231 **Results**

232

Intraclass correlation coefficients and CV demonstrated high within-session reliability for 233 bilateral and unilateral IMTP PF (ICC = .94, CV = 4.7 - 5.5%) (Table 1). Lower reliability 234 235 measures and greater variability were observed for bilateral and unilateral IMTP impulse at time bands (ICC = .81 - .88, CV = 7.7 - 11.8%) (Table 1). Unilateral IMTP left and right IP 236 100 met minimum acceptable reliability criteria (ICC = .83 - .87, CV = 9.3 - 9.5%); however 237 IP 200, IP 250 and IP 300 demonstrated a greater level of variance than has previously been 238 recommended (ICC= .82 - .88, CV = 10.3 - 11.6%).³² Descriptive statistics for bilateral and 239 unilateral IMTP force-time characteristics are presented in Tables 2 and 3. Unilateral IMTP 240 241 descriptive statistics, MSA indexes and ESs are presented in Tables 2 and 3.

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- 243 244

Insert Table 1 around here

245 **Professional Male Rugby League Players**

No significant differences (p > .05, $d \le 0.11$) between right and left limbs were observed for all isometric force-time characteristics; with trivial differences between limbs (Table 2).

248	Conversely, small significant differences (p < .001, $d = 0.27 - 0.46$) were found between D
249	and ND limbs for all isometric force-time characteristics (Table 3).
250	
251	Collegiate Male Athletes
252	No significant differences (p > .05, $d \le 0.32$) between right and left limbs were observed for
253	all isometric force-time characteristics; with trivial to small differences between limbs (Table
254	2). Conversely, small to moderate significant differences (p < .001, $d = 0.43 - 0.91$) were
255	found between D and ND limbs for all isometric force-time characteristics (Table 3).
256	
257	**Insert Table 2 around here**
258	**Insert Table 3 around here**
259	
260	Discussion
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The aims of this study were to assess the within-session reliability of bilateral and unilateral 262 263 stance IMTP force-time characteristics and to determine if significant differences in isometric strength were present between lower limbs in male collegiate and male professional rugby 264 league athletes. The results from this study demonstrated high-within session reliability for 265 bilateral and unilateral stance IMTP PF meeting minimum acceptable reliability criteria. 266 Lower reliability measures and greater variability were observed for unilateral IMTP IP 100, 267 however still met minimum acceptable reliability criteria. Conversely, unilateral IMTP IP 268 200, IP 250 and IP 300 demonstrated a greater level of variance than has previously been 269 recommended (Table 1).³² Trivial to small non-significant differences were observed between 270 force-time characteristics for right and left limbs in collegiate and professional rugby league 271 272 players (Table 2). However, small to moderate significant differences were revealed between D and ND limbs in male collegiate athletes and small significant differences between D and 273 274 ND in professional rugby league players (Table 3). These findings are in agreement with our 275 hypotheses.

The bilateral IMTP has been reported to be highly reliable with a low measurement error.^{24,} 276 ^{25, 27} Traditionally, IMTP assessments have been performed bilaterally, with asymmetries 277 having only been established with the use of dual force platforms during bilateral IMTPs.^{11, 17,} 278 ¹⁸ To our knowledge, this study is the first to investigate a unilateral stance IMTP for the 279 280 assessment of MSA indexes, demonstrating high reliability measures for isometric PF and lower reliability measures for impulse at time bands (Table 1). Further, significant differences 281 were also observed between D and ND limbs (Table 3) for all isometric force-time 282 characteristics. Therefore, this study revealed high within-session reliability for the 283 assessment of unilateral stance IMTP PF and significant differences in force-time 284 characteristics between D and ND limbs in male athletes (Table 3). However, a limitation of 285 the present study is only the within-session reliability of the unilateral stance IMTP force-286 287 time characteristics was assessed, therefore, further research is required assessing between session test-retest reliability of the unilateral stance IMTP. 288

289

As previously stated limited studies have inspected unilateral multi-joint isometric strength through unilateral isometric squat assessments.^{13, 22, 23} Hart et al²² reported very high reliability measures of unilateral squat isometric PF (ICC = .96 - .98, CV = 3.6 - 4.7%) in 11 male athletes. Spiteri et al²³ demonstrated similar reliability measures for unilateral isometric squat PF (ICC = .95, CV = 5.5 - 7%) in 12 male and 12 female athletes. Specifically, the

present study demonstrated comparable reliability measures for unilateral IMTP PF (ICC = 295 .94, CV = 4.7 - 5.0%) to the above-mentioned studies in a large male sample (n = 54). 296 Moreover, athletes may experience less discomfort when performing a unilateral IMTP in 297 comparison to a unilateral isometric squat, due to pulling an immovable bar in comparison to 298 pushing against an immovable bar positioned on the upper back (mid trapezius) during 299 isometric squats. Consequently, the unilateral stance IMTP demonstrates high within-session 300 reliability for PF assessments, with further research required into the between session 301 reliability of unilateral PF. 302

This study is the first to inspect impulse at time bands (0-100, 0-200, 0-250, 0-300 ms) during 303 unilateral stance IMTP assessments, demonstrating lower within-session reliability (ICC = 304 .82 - .88, CV = 9.3 - 11.6%) and greater variability in contrast to PF reliability measures. 305 Excluding IP 100, all unilateral stance impulse at time bands demonstrated a greater level of 306 variance than has previously been recommended. ³² Dynamic tasks such as sprinting, jumping 307 and changing direction are heavily dependent on an athlete's capability to rapidly apply 308 unilateral force over short time intervals;^{23, 27} therefore the ability to assess an athlete's 309 unilateral force and impulse production capabilities via the unilateral stance IMTP may allow 310 practitioners and scientists to identify any deficiencies in force production in specific limbs 311 and also monitor the effectiveness of training interventions. Although it should be 312 313 acknowledged that isometric and dynamic tasks are different. Our results indicate that the unilateral IP 100 demonstrates acceptable reliability, although practitioners should be aware 314 315 greater variability may be observed when assessing impulse at alternative time bands (Table 316 1).

No significant differences were observed between left and right limbs for isometric forcetime characteristics in collegiate male athletes (p > .05, $d \le 0.32$) and professional rugby league players (p > .05, $d \le 0.11$). However, significant differences were observed when comparing D and ND limbs in male collegiate athletes (p < 0.001, d = 0.43 - 0.91) and professional rugby league players (p < .001, d = 0.27 - 0.46); highlighting that isometric strength deficits between lower limbs are present in male athletes. Future research is required establishing isometric MSA indexes in female athletes.

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325	**Insert Figure 1 around here**
326	**Insert Figure 2 around here**

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- 328

The magnitudes of asymmetry in collegiate male athletes (6.2 \pm 4.8 to 11.5 \pm 9.5%) and 329 professional rugby league players $(5.1 \pm 3.8 \text{ to } 9.6 \pm 8.6\%)$ are presented in Table 3; 330 331 individual PF imbalances are also illustrated in Figures 1 and 2. It should be noted that the that larger asymmetry values observed in the collegiate male athletes could be attributed to a 332 heterogonous mixed sporting sample that contained athletes from sports where there are 333 specific asymmetrical movement demands for example soccer, boxing and cricket which may result in the development of strength asymmetries.^{34, 35} For example, Figure 2 illustrates the 334 335 individual PF imbalance between D and ND limbs in collegiate male athletes, showing the 336 337 boxers in this cohort demonstrated higher asymmetries in contrast to the other athletes from different which elevates the mean imbalance of this cohort. It should also be acknowledged 338 the results of this present study are only applicable and representative of the athletes at the 339 340 specific time of the season they were tested; and are therefore likely to change over a competitive season. Researchers have shown seasonal changes in fitness and strength characteristics throughout a season^{36, 37} and the specific training phase has also shown to influence jump performance.³⁸ However, to our knowledge no literature exists investigating isometric strength asymmetries throughout a competitive season. Therefore, a future direction of research is to investigate seasonal variations in MSA as measured by the IMTP.

A strength discrepancy of 10-15% between limbs is considered to represent a potentially problematic asymmetry.² Although, no literature is available to substantiate this claim,⁸ it is likely that the typical magnitude of MSA may vary between different muscle strength qualities for example concentric, eccentric, isometric and dynamic strength,^{14, 15} and between different athlete populations.³⁵ Our findings provide normative MSA data for unilateral IMTP kinetics in different populations (Table 3). Athletes who demonstrate MSA greater than the values in Table 3 could therefore be considered asymmetrical.

353

354 Asymmetries during IMTP have only been established bilaterally with each foot on a separate force plate, with researchers observing asymmetries in isometric force time-characteristics in 355 male and female athletes.^{11, 17-19} Further, research suggests that weaker athletes display 356 greater asymmetries in isometric force-time characteristics in comparison to stronger athletes 357 during bilateral IMTPs^{17, 18} and bilateral isometric squats¹⁶ which may have a detrimental 358 impact on vertical jumping performance.¹¹ Block periodised bilateral strength training has 359 been reported to reduce bilateral asymmetries in weaker athletes;¹⁶ highlighting the 360 importance of maximising athletes bilateral strength to reduce the magnitude of bilateral 361 MSA. It is unknown if this would be the case for unilateral IMTP MSA, thus future 362 investigations are required determining the impact of strength training on unilateral IMTP 363 364 MSA.

365

It should be noted that above-mentioned studies have inspected asymmetries during bilateral 366 isometric squats and IMTPs and is therefore not a direct assessment of an isolated limb's 367 force production capabilities. Consequently, a unilateral stance IMTP would allow the direct 368 assessment of multi-joint isometric force production of a specific limb replicating unilateral 369 stance of sprint, jumps and COD supported by the high reliability shown in the current 370 findings. This will also help scientists and practitioners assess strength deficits between limbs 371 and identify normative MSA values for athletic populations to benchmark standards in 372 monitoring and strength assessments. Further, from a rehabilitation perspective a unilateral 373 stance IMTP could be implemented to assess an athlete's isometric strength pre- and post-374 injury to determine the effectiveness training interventions and establish return to play 375 criteria. 376

377

The impact of MSA on injury risk in athletes remains inconclusive;⁸ however from a performance perspective it would be advantageous to be equally proficient in force production between limbs,¹⁴ due to the unilateral requirements of sprinting, jumping, landing and change of directions. Previous studies have shown strength deficits between limbs can negatively impact performance during change of direction,¹⁰ vertical jumping,^{11, 12} and kicking.¹³ Our results revealed significant differences in unilateral IMTP force-time characteristics between D and ND limbs in male athletes. However the implications of unilateral IMTP MSA on dynamic performance such as jumping and COD is unknown, thusis an area of further research.

387

388 **Practical Applications**

Overall, this study confirmed that the unilateral stance IMTP produces high within-session 389 reliability for PF and IP 100 also met minimum reliability criteria. Furthermore, small to 390 moderate significant differences were observed between D and ND limbs for all isometric 391 force-time characteristics with greater magnitudes of asymmetry of MSA in male collegiate 392 athletes in comparison to professional rugby players. Male athletes with isometric force-time 393 characteristics asymmetries greater than the mean plus the SD of the normative MSA indexes 394 presented in Table 3 maybe considered asymmetrical. Practitioners and scientists should 395 therefore consider assessing athlete's unilateral isometric force production capabilities via a 396 unilateral stance IMTP. This would permit the direct assessment of multi-joint isometric 397 398 force production of the lower limbs replicating the unilateral stance of sprinting, jumping and COD; allowing practitioners to identify strength deficits between limbs so subsequent 399 training programmes can be implemented to reduce the deficit which may reduce the 400 likelihood of injury and improve athletic performance. From a rehabilitation perspective a 401 402 unilateral stance IMTP would allow comparisons of lower limb strength and pre- and postinjury and also monitor the effectiveness of training interventions. 403

404 Conclusion

405 Bilateral and unilateral stance IMTP assessments demonstrated high within-session reliability for PF and lower although acceptable reliability measures for IP 100. Impulse at time bands 406 (0-200, 0-250 and 0-300 ms) demonstrated a greater level of variance than has previously 407 408 been recommended. No significant differences were observed between left and right limbs during unilateral stance IMTP for male collegiate and rugby league players however 409 significant differences were revealed for all isometric force-time characteristics between D 410 and ND limbs. Future research should focus on the effect of strength training on the 411 magnitude of unilateral stance IMTP asymmetry and effect of isometric MSA on athletic 412 performance. 413

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