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Woolley, Sandra and Rukasha, Tendai and Kyriacou, Theocharis and Collins, Timothy (2020) Evaluation of Wearable Electronics for Epilepsy: A Systematic Review. *Electronics (Basel)*, 9 (6). p. 968. ISSN 2079-9292

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Version: Published Version

Publisher: MDPI AG

DOI: <https://doi.org/10.3390/electronics9060968>

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Review

Evaluation of Wearable Electronics for Epilepsy: A Systematic Review

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Received: 25 May 2020; Accepted: 8 June 2020; Published: 10 June 2020

Abstract: Epilepsy is a neurological disorder that affects 50 million people worldwide. It is characterised by seizures that can vary in presentation, from short absences to protracted convulsions. Wearable electronic devices that detect seizures have the potential to hail timely assistance for individuals, inform their treatment, and assist care and self-management. This systematic review encompasses the literature relevant to the evaluation of wearable electronics for epilepsy. Devices and performance metrics are identified, and the evaluations, both quantitative and qualitative, are presented. Twelve primary studies comprising quantitative evaluations from 510 patients and participants were collated according to preferred reporting items for systematic reviews and meta-analyses (PRISMA) guidelines. Two studies (with 104 patients/participants) comprised both qualitative and quantitative evaluation components. Despite many works in the literature proposing and evaluating novel and incremental approaches to seizure detection, there is a lack of studies evaluating the devices available to consumers and researchers, and there is much scope for more complete evaluation data in quantitative studies. There is also scope for further qualitative evaluations amongst individuals, carers, and healthcare professionals regarding their use, experiences, and opinions of these devices.

Keywords: wearable electronics; epilepsy; seizure detection; smart watch; systematic review

1. Introduction

Epilepsy is a neurological disorder affecting 50 million people worldwide [1]. While seizures can be controlled with antiepileptic drugs, more than 30% of people with epilepsy have drug-resistant seizures [2]. The timely detection of seizures is important in hailing assistance that can reduce the potential for injuries and sudden unexpected death in epilepsy (SUDEP) events [3,4]. This paper reviews the literature relevant to qualitative and quantitative assessments of the wearable electronics available to individuals and researchers for the detection of epilepsy seizures.

The onset of epileptic seizures is associated with autonomic changes including flushing, sweating, and heart rate changes [5,6] that have the potential to be detected by wearable temperature, electrodermal activity (EDA), and optical pulse “photoplethysmography” (PPG) sensors, respectively. The seizures themselves can be convulsive or nonconvulsive. Convulsive seizures involve repeated involuntary contractions and relaxations of muscles that appear as repetitive, rhythmic, shaking motions. The pronounced motor activity of convulsive seizures makes them potentially recognisable with accelerometry. In contrast, nonconvulsive seizures can be difficult to detect; they can appear as simple absences or losses in muscle strength. Seizure types are described

according to their type of presentation as tonic, clonic, tonic-clonic, myoclonic, atonic, and absence as summarised below:

- Tonic seizures (TS) associated with contractions of the muscles;
- Clonic seizures (CS) associated with repeated contractions and relaxation of muscles;
- Tonic-clonic seizures (TCS) associated with stiffening followed by shaking;
- Myoclonic seizures (MS) associated with twitching regions of muscles;
- Atonic seizures associated with loss of muscle strength;
- Absence seizures associated with individuals appearing detached or inattentive.

The management and treatment of epilepsy relies on the assessment of seizure presentation and frequency, but patient self-reports and carer recall can be unreliable [7] and patient seizure diaries can underestimate seizure frequency [8,9]. In a review of electroencephalography (EEG) and other seizure reporting technologies for epilepsy treatment, Bidwell et al. [10] highlighted “a strong need for better distinguishing between patients exhibiting generalized and partial seizure types as well as achieving more accurate seizure counts” but concluded that high false positive seizure detection rates meant that most technologies failed to surpass patient self-reporting performance.

Whilst EEG is used in clinical laboratory settings for seizure assessment and diagnosis, new research toward wearable ambulatory EEG sensing [11] offers future opportunities for assessment and monitoring beyond the clinical environment. However, currently, despite “great interest in the use of wearable technology across epilepsy service users, carers, and healthcare professionals” [7], the monitoring of seizures outside the clinic, in real-world settings and during the activities of everyday living, is limited to the sensing afforded by a small set of available wearable epilepsy seizure-sensing devices. Additionally, some nonwearable devices are available, for example, sensors designed to attach to a bed or mattress to detect night-time seizures; however, the focus of this review is on wearable devices.

Wearable Electronics for Epilepsy Seizure Detection

There has been strong interest and market growth in wrist-worn wearable health and well-being devices [12] incorporating digital thermometers for temperature, conductivity sensors for EDA, micro-electromechanical systems (MEMS) for accelerometry, and light-emitting diodes (LEDs) and photodiodes for PPG pulse wave detection [13], as well as new advances toward flexible skin-inspired sensors [14]. Despite reliability concerns related to ambulatory sensing [15], wearable devices are increasingly used in clinical and healthcare applications. Low- and mid-range wearable devices typically comprise optical PPG pulse, EDA, temperature, and three-axis accelerometer sensors [16–19]. As illustrated in Figure 1, wearable electronics for epilepsy seizure detection, based on wrist- and arm-worn sensor configurations, are now available to individuals and researchers for the purpose of detecting and reporting seizures and alerting carers for timely assistance. Additional sensors such as gyroscopes and GPS (global positioning system) receivers can detect rotational movements and location, respectively. Signals from these sensors can be used to detect “preictal” periods before a seizure by electrodermal activity and heart rate changes, or, during the seizure, shaking motor movements (or lack of movement during absences), and can be used to locate, report, and log seizure events. It is, however, difficult to reliably detect seizures in everyday life [20], and the challenge of disambiguating seizures and normal everyday (seizure-like) movements such as teeth brushing may result in false alarms that require repeated cancellations and which may disincentivise uptake among patients.

Table 1 summarises the currently available wearable consumer seizure-detecting devices that have been evaluated in the literature. These include the Embrace seizure-detecting wrist-worn sensor, developed by Empatica [21]. Embrace is a maturing product that is available to consumers via device purchase and monthly subscription (subscriptions, at the time of writing, are £9.90–£44.90 per month). Empatica also market an “E4” (previously “E3”) research version of their Embrace device that provides researchers with access to the raw sensor data that can be used to test seizure-detecting algorithms. Also, as shown in Table 1, other devices reported in the literature include the Epi-Care

free [22], NightWatch [23], and SmartWatch [24]. Epi-Care free is a wrist-worn (or ankle-worn) sensor incorporating an accelerometer, gyroscope, and GPS to detect seizure motor activity and send alerts to family members or telecare services (subscriptions, at the time of writing, are £995 and £1115 per year). The NightWatch sensor is an armband wearable that senses pulse and activity to detect and report nocturnal seizures. The Smart Monitor SmartWatch is a seizure detector that makes use of wearable heart rate and activity data (originally from prototype wearable devices and now the app, named “Inspyre”, can access data from compatible Apple and Samsung Galaxy and Gear watches) and summon help to the GPS location of the wearer (subscriptions, at the time of writing, are from £9.99 to £24.99 per month). Other wearable consumer products for epilepsy seizure detection include Brio, Epilert (no longer available), Pulse Companion, and Open Seizure Detector (App). However, these devices have not been assessed in the literature.

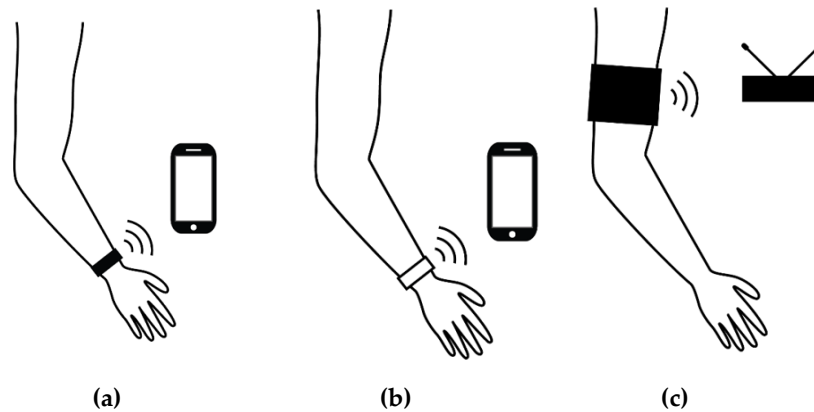


Figure 1. Wearables and apps for epilepsy seizure detection: (a) dedicated wrist-worn sensing device and companion app (e.g., Embrace and Epi-Care free); (b) app using sensed data from a compatible consumer wrist-worn tracker (e.g., the SmartWatch Inspyre app with an Apple or Samsung device); (c) a non-wrist wearable with a base station (NightWatch).

Table 1. Wearable electronics for epilepsy seizure detection.

Device	Sensors	Manufacturer/Supplier	Software/Applications	Hardware/Platform
Embrace/Embrace 2 E4	Accelerometer PPG Temperature EDA Gyroscope (Embrace 2)	Empatica Inc./Srl (Boston, USA/Milan, Italy)	Alert App Mate App	Apple/Android Smartphone
Epi-Care free	Accelerometer Gyroscope	Danish Care Technology ApS (Sorø, Denmark)	Epi-Care App	Apple/Android Smartphone
NightWatch	Accelerometer PPG	LivAssured B.V. (Leiden, The Netherlands)	NightWatch online portal	Dedicated base station
Smart Monitor (SmartWatch/ Inspyre App)	Accelerometer PPG	Smart Monitor (San Jose, USA)	Smart Monitor App Web Portal	Apple/Android Smartphone and compatible Samsung and Apple Watches

Detection Performance

Figure 2 summarises seizure detections in terms of true/false and positive/negative outcomes and the related sensitivity, specificity, positive predictive value (PPV), and negative predictive value (NPV), and the associated formulae, including the false alarm rate (FAR), are summarised in Equations (1)–(6).

		Epileptic seizure		
		Condition positive	Condition negative	
Wearable seizure detection	Seizure detection positive	True Positive (TP)	False Positive (FP)	Positive predictive value (PPV) = TP/(TP + FP)
	Seizure detection negative	False Negative (FN)	True Negative (TN)	Negative predictive value (NPV) = TN/(FN + TN)
		Sensitivity = TP/(TP + FN)	Specificity = TN/(FP + TN)	

Figure 2. Seizure detection performance metrics.

$$\text{Sensitivity} = \text{TP}/(\text{FN} + \text{TP}) \quad (1)$$

$$\text{Specificity} = \text{TN}/(\text{TN} + \text{FP}) \quad (2)$$

$$\text{Positive Predictive Value (PPV)/Precision} = \text{TP}/(\text{TP} + \text{FP}) \quad (3)$$

$$\text{Negative Predictive Value (NPV)} = \text{TN}/(\text{FN} + \text{TN}) \quad (4)$$

$$\text{Accuracy} = (\text{TP} + \text{TN})/(\text{TP} + \text{TN} + \text{FP} + \text{FN}) \quad (5)$$

$$\text{False Alarm Probability} = \text{FP}/\text{day} \quad (6)$$

Ideally, assessments of wearable devices would present results for these metrics for significant numbers of subjects over sufficient duration for testing detection of a substantial number of seizures of different types. In addition, assessments would also ideally support repeatability by clearly specifying test conditions, device models, and, also, version information [25]. Given the importance of timely alerts for seizure detection and the need to reduce the anxiety and alarm fatigue associated with high false alarm rates (FARs), detection latency and FARs should also be reported.

2. Method

A systematic review of primary studies evaluating wearable seizure-detecting devices spanning almost fifteen years (from 1 January 2005 to 31 October 2019, when the review was initiated) was conducted with an evidence-based methodology [26,27] and in accordance with PRISMA guidelines

[28]. A requirement of the review was that devices were identified and available to individuals or researchers (i.e., not unavailable, proof-of-concept, laboratory prototypes).

2.1. Search Strategy

Both technology and medical digital libraries were used to identify primary studies. These were Association for Computing Machinery (ACM), Institute of Electrical and Electronics Engineers (IEEE) Xplore Digital Library, Medline, ScienceDirect, and Wiley Online Library.

The keyword search string below was evolved to identify primary studies relevant to wearable epilepsy sensing devices:

("wearable" OR "smart watch" OR "smart watch" OR "wrist-worn" OR "wrist worn" OR "wrist worn" OR "wristband" OR "armband") AND ("epileptic" OR "epilepsy").

2.2. Eligibility Criteria and Selection

Studies were eligible for selection if they met all three of the following inclusion criteria:

1. Primary studies in peer-reviewed literature;
2. Studies where the main theme is consumer wearable electronics for epilepsy seizure detection;
3. Studies reporting quantitative and/or qualitative assessment data.

The relevant papers were assessed for quality according to screening criteria including rigour, credibility, and relevance [29].

3. Results

Following the PRISMA systematic review guidance outlined in Figure 3, a total of 12 papers satisfied the eligibility criteria. A second researcher checked the screening and eligibility of papers and a third researcher moderated the results.

As summarised in Table 2, all 12 studies reported qualitative assessments (8 conducted in clinical settings and 4 in free-living conditions). Two of the 12 studies also reported quantitative assessments. While the search process did initially identify qualitative papers on wearable devices for epilepsy, some of these studies [30,31] were assessments of perceptions about the potential of such devices rather than assessments of actual use. No studies reported solely qualitative assessment data for the real use of available wearable devices for seizure detection.

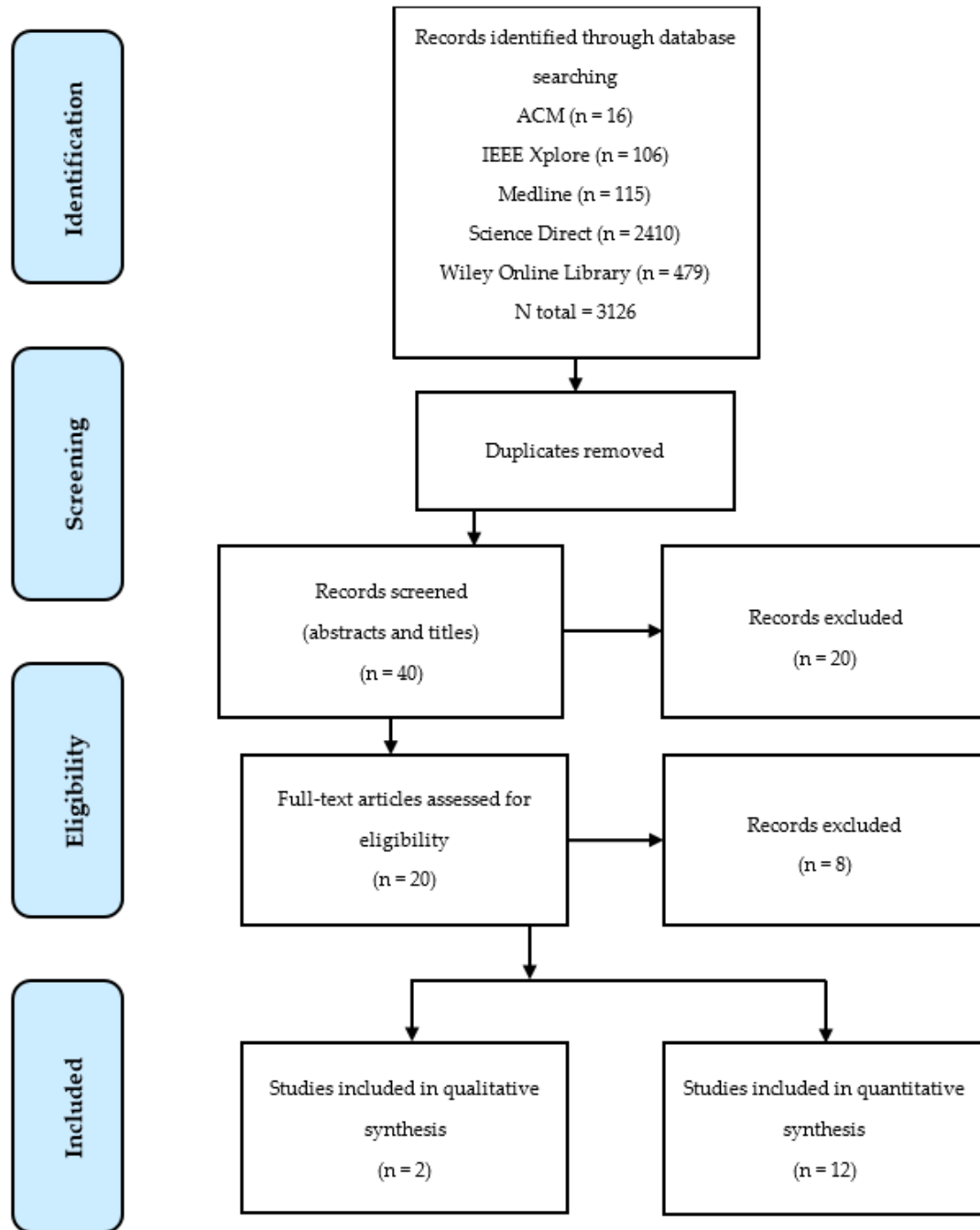


Figure 3. Flow diagram of the systematic review according to preferred reporting items for systematic reviews and meta-analyses (PRISMA) guidelines.

Table 2. Overview of studies and participant numbers.

No. Studies = 12		
No. Quantitative = 12		No. Qualitative = 2
Clinical setting = 8	Free-living = 4	-
No. participants/patients = 341	No. participants/patients = 169	No. participants/patients = 104
TOTAL = 510		TOTAL = 104

3.1. Quantitative Studies

3.1.1. Clinical Setting

Eight of the 12 quantitative studies were conducted in clinical settings. All eight were evaluation studies [32–39] with data gathered from epileptic inpatients and outpatients; none were two-arm or controlled studies with healthy participants. Most studies compared recorded device data with other clinical reference recordings, including EEG, video EEG (vEEG), electromyography (EMG), and electrocardiogram (ECG). The studies are summarised in Table 3 in terms of the devices used, the numbers of participants, the numbers of seizures detected, and, where specified, the study duration. As shown in the summary in Table 3, four of the studies used Empatica E3, E4, and Embrace devices, three used Smart Monitor’s evolving SmartWatch devices, and one used the Epi-Care free. The numbers of patient participants varied from 3 to 135. A study [33] with three participants selected 1 h recorded segments rather than continuous recordings. Otherwise, observation durations varied within studies [33,38,39] as well as between studies from 17 h to 487 days, and two studies [35,37] did not report durations. The total number of seizures detected in studies varied from 7 and 55 and, across all studies, a total of 226 seizures were reported as detected. Only one study [33] did not report the number of detected seizures.

Table 4 summarises the performance assessments of the studies. The reporting of performance metrics was variable and sparse across most of the studies. For example, false alarm rates for only three studies could be identified. The studies using the Empatica E3 and E4 implemented machine learning detection methods (kNN: k-nearest neighbour; RF: random forest; NB: naïve Bayes; SVM: support vector machine). Regalia et al., 2019 [35] made brief reference to previously unpublished assessments with 135 patients and 22 seizures with 100% sensitivity and an FAR of 0.42 per day for a “fixed and frozen” algorithm. No methodology, sensitivity, or other assessment information was provided, and the paper largely focused on compiling and comparing other Empatica wristband performance indicators. Heldberg et al., 2015 [32] reported the sensitivity and specificity for two different classifiers. Vandecasteele et al. [34] compared the performance of SVM classifiers on hospital ECG with wearable ECG and E4 PPG recordings. PPG motion artefacts (which would have been largely induced by the seizures themselves) made more than half of the seizures undetectable via this approach and resulted in a poor sensitivity of 32%. The studies encompassed different seizure types but with TCS and “motor” seizures often included. Dramatically different performance results were observed. For example, sensitivities of 100% and 16% were reported by the authors of [35] and [37], respectively. Notably, the latter paper [37] comprised a large number of (undetected) nonmotor seizures. The levels of patient activity and any movement constraints were not generally explicitly reported and, in any case, are difficult to convey. However, in the clinical setting, worn sensors usually benefit from reduced interference from activities of daily living. For example, the good wearable performance for the small study in [33] was achieved from recordings taken simultaneously with EEGs, i.e., when one would expect patients to be inactive.

Table 3. Clinical setting studies with number of seizures and duration.

Clinical Settings				
Study	Device	No. Participants	No. Seizures Detected	Duration
Heldberg et al., 2015 [32]	E3	8	55	23 days
Al-Bakri et al., 2018 [33]	E4	3	unspecified	4–5 days (1 hour intervals)
Vandecasteele et al., 2017 [34]	E4	11	47	29 days
Regalia et al., 2019 [35]	Embrace and E4	135	40	unspecified
Lockman et al., 2011 [36]	SmartWatch	40	7	487 days
Patterson et al., 2015 [37]	SmartWatch	41	30	unspecified
Velez et al., 2016 [38]	SmartWatch	30	12	1–9 days
Beniczky et al., 2013 [39]	Epi-Care free	73	35	17–171 hours
-	-	TOTAL = 341	TOTAL = 226	-

Smart Monitor’s SmartWatch was used in three of the eight clinical assessments. Patterson et al. [37] reported the lowest sensitivity (16% overall: 31% for general tonic-clonic (GTC) and 0% for MS) in a study of 41 patients aged 5–41 years. Citing Lockman et al. [36], the authors did not record false positives “because these are well known”. Lockman et al. [36] did report 204 false alarm occurrences in their SmartWatch study with 40 patients between “March 2009 and June 2010” but did not specify an FAR or confirm the duration of actual usage within the study period. Velez et al. [38] referred to 81 false alarms but also did not specify an FAR (and one cannot be estimated because of the varying durations of 1–9 days). Beniczky et al. [39] reported a sensitivity of 90% and an FAR of 0.2 per day in a study with 73 participants with GTC seizures who were monitored for 17–171 hours. An average detection latency of 55 s was reported.

Table 4. Performance assessments in clinical settings.

Authors/ No. Participants	Device	Seizure	Sensitivity	Specificity	FAR	PPV/R	Detection Latency
Heldberg et al., 2015 [32] 8 participants	E3	PNMS, PMS	89.1% (kNN) 87.3% (RF)	93.1% (kNN) 95.2% (RF)	-	-	-
Al-Bakri et al., 2018 [33] 3 participants	E4	-	84% (NB) (preictal sleep) 78% (NB) (preictal wake)	79% (NB) (preictal sleep) 80% (NB) (preictal wake)	-	-	-
Vandecasteele et al., 2017 [34] 11 participants	E4 (PPG)	TLS, CPS	32% (SVM)	-	1.80 per hour	1.43%	-
Regalia et al., 2019 [35] 135 participants	E4 and Embrace	GTC	100%	-	0.42 per day	-	-
Lockman et al., 2011 [36] 40 participants	SmartWatch	TCS	87.5%	-	-	-	-
Patterson et al., 2015 [37] 41 participants	SmartWatch	TS, GTC, MS, MTS, PS	16%	-	-	-	-
Velez et al., 2016 [38] 30 participants	SmartWatch	TCS	92.3%	-	-	-	-
Beniczky et al., 2013 [39] 73 participants	Epi-Care free	TCS	90%	-	0.2 per day	-	55 s

Seizure Abbreviations: CPS: complex partial seizures, GTC: general tonic-clonic, MS: myoclonic seizures, MTS: myoclonic-tonic seizures, PMS: predominantly motor seizures, PNMS: predominantly nonmotor seizures, PS: partial onset seizures, TCS: tonic-clonic seizures, TLS: temporal lobe seizures, TS: tonic seizures. Classifier Abbreviations: kNN: k-nearest neighbour; NB: naïve Bayes; RF: random forest; SVM: support vector machine. Other Abbreviations: FAR: False Alarm Rate; PPV/R: Positive Predictive Value/Rate.

3.1.2. Free-Living Environment

Four of the 12 quantitative studies report free-living environment evaluations. These studies are summarised in Tables 5 and 6 and comprise 169 participants and 850 seizures.

Table 5. Free-living studies with number of seizures and duration.

Free-Living Settings				
References	Device	Participants	No. Seizures Detected	Duration
Onorati et al., 2017 [40]	E3 and E4	69	32	247 days
Van de Vel et al., 2014 [3]	Epi-Care free	1	9	19 nights
Meritam et al., 2018 [8]	Epi-Care free	71	-	15 months median (24 days to 6 years)
Arends et al., 2018 [41]	NightWatch	28	809	1826 nights
-	-	TOTAL = 169	TOTAL = 850	-

Onorati et al. [40] reported a range of classifier performances for the E3 and E4 with sensitivities from 83.64% to 94.55% and FARs of between 0.2 and 0.29 per day. Van de Vel et al. [3] and Meritam et al. [8] both reported Epi-Care free evaluations with 71 and 1 participants, respectively. For the 71 patients [8], a sensitivity of 90% and an FAR of 0.1 per day were reported. Arends et al. [41] reported a sensitivity of 86% for the NightWatch arm-worn nocturnal seizure monitor, an FAR of 0.25 per night, and a PPV of 49%.

Table 6. Performance metrics in a free-living setting.

Study/No: of Participants	Device	Seizure	Sensitivity	Specificity	FAR	PPV/R	Detection Latency
Onorati et al., 2017 [40] 69 participants	E3 and E4	BTCS, FTC	83.64% (Classifier I)	-	0.29 per day (Classifier I)	-	31.2 s (Classifier I)
			92.73% (Classifier II)		0.21 per day (Classifier II)		29.3 s (Classifier II)
			94.55% (Classifier III)		0.20 per day (Classifier III)		29.3 s (Classifier III)
Van de Vel et al., 2014 [3] 1 participant	Epi-Care free	TS, CS, TCS	41%	-	0.05 per night	-	-
Meritam et al., 2018 [8] 71 participants	Epi-Care free	BTCS	90% BTCS median	-	0.1 per day median	-	-
Arends et al., 2018 [41] 28 participants	NightWatch	MS, TC, TCS, Hyperkinetic	86% median	-	0.25 per night median	49% median	-

Seizure Abbreviations: BTCS: bilateral tonic-clonic seizures, CS: clonic seizures, FTC: focal tonic-clonic, FS: focal seizures, MS: myoclonic seizures, TCS: tonic-clonic seizures, TS: tonic seizures. Other Abbreviations: FAR: false alarm rate, PPV/R: positive predictive value/rate.

3.1.3. Data Failures—Missing and Unusable Data

In addition to missed seizures caused by algorithms failing to detect seizures in acquired data, seizures can also be missed when data are not recorded, not received, or not usable (for example, if they are so corrupted as to be unusable). There were limited discussions of data failures or the “missingness” of data in the studies. Examples are summarised in Table 7.

Table 7. Missing data.

Studies	Device	Participants	Data Failures	Reasons
Vandecasteele et al., 2017 [34]	E4	11	PPG motion artefacts	Motion artefacts “PPG signal was drastically affected ... 55% of the seizures could not be detected because of motion artefacts ... no reliable HR could be extracted”
Velez et al., 2016 [38]	SmartWatch	30	3 occasions	2× wireless communication failures and 1× device not worn during seizure
Beniczky et al., 2013 [39]	Epi-Care free	73	“15 times”	“Device deficiencies” (including 2× “technical error”, 11× “battery failure”)

3.2. Qualitative Studies

Only two studies provided qualitative assessment data for device evaluations. Both of these studies also reported quantitative evaluations that were included in the earlier sections. Summaries of patient and stakeholder views and observations are listed in Table 8.

Table 8. Qualitative studies.

Study/ No. Participants	Stakeholder Views and Observations	
	Benefits	Barriers/Concerns
Arends et al., 2018 [41] 33 qualitative carer respondents	<ul style="list-style-type: none"> Timely responses to urgent situations. Offers carers more freedom. Helps carers give better care. More autonomy for people with epilepsy. 	<ul style="list-style-type: none"> Skin irritation. Armband not fitting properly. Poor signal reception.
Meritam et al., 2018 [8] 71 qualitative patient respondents	<ul style="list-style-type: none"> Good overall device satisfaction (5.5/7) Easy to use. Clear alarm signals. Timely alerts enabled 40% reduction in injuries. Feeling of security and a decreased psychological burden. 	<ul style="list-style-type: none"> High false alarm rate. Skin irritation or discomfort. Low effectiveness for detecting seizures. Unstable sensor communication and interference issues. Limited battery life and lack of water resistance. 10% of patients stopped using the device for device-related reasons.

Arends et al., 2018 [41] evaluated the NightWatch night-time upper arm seizure monitor using a multifactor questionnaire with 33 carer stakeholder respondents comprising 30 nurses, 2 parent carers, and 1 “not specified”. Meritam et al., 2018 [8] performed a qualitative evaluation of the Epi-

Care free monitor with 71 patient participants aged 7–72 years using a post-study systems usability questionnaire (PSSUQ) comprising 13 questions and requiring a 1–7 Likert-scale response from participants on aspects on monitor usability.

Both studies identified concerns in terms of (a) physical intrusion, e.g., discomfort or irritation, and (b) performance concerns, e.g., signal reception or detection failures. Participants in both studies agreed with the benefits of the monitors in terms of the potential for improved responses to seizure events and the potential for improved care outcomes.

4. Discussion

The aim of this review was to collate and analyse qualitative and quantitative assessments of wearable electronics for epilepsy seizure monitoring that are available to individuals and researchers. Although there are over 3000 works in the literature discussing, proposing, and evaluating novel and incremental approaches to epilepsy seizure detection, there are very few that report evaluation data and, as observed previously [42], none that report comparative results of large-scale studies. In terms of the Oxford Centre for Evidence-Based Medicine 2011 Levels of Evidence 1–5 scale [43], none of the reviewed studies would qualify as the highest level of evidence (Level 1), and most would rank as Level 3 or below.

The diversity of the reviewed studies in terms of motor and nonmotor seizure types and levels of patient activity/freedom of movement is matched by the diversity of results including, for example, very high and very low sensitivities.

Across the reviewed works there was a lack of full detail, including details required to establish important metrics such as false alarm rates (FARs) and details important to reproducibility such as device, firmware, and app version numbers [44]. Ideally, the frequency, duration, impact, and cause of all data recording failures (resulting in the “missingness” of data) would also be provided in all performance assessment studies. There was also a lack of detail regarding the performance of the devices themselves in terms of seizure detection and estimation of key parameters such as heart rate. In a recent study [45], researchers compared consumer-grade and research-grade heart rate (HR) and heart rate variability (HRV) estimating wearables (including the Empatica E4 and two other HR sensing devices) and observed that “while the research-grade wearables are the only wearables that provide users with raw data that can be used to visualize PPG waveforms and calculate HRV, the HR measurements tended to be less accurate than consumer-grade wearables. This is especially important for researchers and clinicians to be aware of when choosing devices for clinical research and clinical decision support.” [45] This very difficult problem of achieving accurate and reliable continuous sensor data in nonsedentary scenarios is highly significant and worthy of more attention if researchers are to develop robust methods and make valid conclusions from acquired data.

Wearable electronic devices for epilepsy seizure detection have the potential to improve patient outcomes and to afford carers more freedom. However, the technology is still evolving. There are opportunities for improvements in system reliability and algorithm detection performance and, ideally, monitors would be sensitive across the range of seizure types whilst maintaining acceptably low false alarm rates. Ideally, future seizure sensing systems and algorithms would benefit from detailed qualitative and quantitative assessments of their performance. However, we should appreciate that assessing technology in critical health scenarios is not easy. Clinical assessments are onerous and resource-expensive undertakings, and their timescales are at odds with the iterative updating of digital technologies. Free-living assessments in particular require investments in time and resources, and they present additional difficulties in terms of truth data.

5. Conclusions

There is much scope for further research and improved performance reporting of wearable devices for epilepsy seizure detection and monitoring. There is a lack of qualitative studies eliciting feedback and stakeholder recommendations from real-world experiences of device usage. Ideally, future studies will report on the data quality and reliability of the sensing devices and provide much

more detailed information regarding assessments, including device model and version numbers as well as detailed contextual information about the wearers and their activity.

Author Contributions: Conceptualisation, T.K., T.R.; methodology, T.K., T.R., S.I.W.; formal analysis, T.R.; investigation, T.R., T.C. and S.I.W.; writing—original draft preparation, T.R., S.I.W.; writing—review and editing, T.R., S.I.W., T.C.; visualisation, T.C. and S.I.W.; project administration, T.K. and S.I.W. All authors have read and agreed to the published version of the manuscript.

Funding: This research received no external funding.

Acknowledgments: Tendai Rukasha thanks Evaresto Rukasha and Betty Rukasha for PhD funding and thanks Pearl Brereton for her comments and suggestions.

Conflicts of Interest: The authors declare no conflict of interest.

Abbreviations

The following abbreviations are used in this manuscript:

BTCS	Bilateral tonic-clonic seizures
CPS	Complex partial seizures
CS	Clonic seizures
ECG	Electrocardiogram
EDA	Electrodermal activity
EMG	Electromyography
FN	False negative
FNV/R	False negative value/rate
FP	False positive
FPV/R	False positive value/rate
FS	Focal seizures
FTC	Focal tonic-clonic
GTC	General tonic-clonic
HRV	Heart rate variability
kNN	k-nearest neighbour
MS	Myoclonic seizures
MTS	Myoclonic-tonic seizures
NB	Naïve Bayes classifier
NPV/R	Negative predictive value/rate
PMS	Predominantly motor seizures
PNMS	Predominantly non-motor seizures
PPG	Photoplethysmography
PPV/R	Positive predictive value/rate
PRV	Pulse rate variability
PS	Partial onset seizures
RF	Random forest
SUDEP	Sudden unexpected death in epilepsy
SVM	Support vector machine
TCS	Tonic-clonic seizures
TLS	Temporal lobe seizures
TN	True negative
TP	True positive
TPV/R	True positive value/rate
TS	Tonic seizures
vEEG	Video electroencephalogram

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