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1 **Motor development in infancy and spine shape in early old age: findings from a British**
2 **birth cohort study**

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51 **Abstract:**

52 Spine shape changes dramatically in early life, influenced by attainment of developmental
53 milestones such as independent walking. Whether these associations persist across life is
54 unknown. Therefore, we investigated associations between developmental milestones and
55 spine shape, as determined using statistical shape models (SSMs) of lumbar spine from DXA
56 scans in 1327 individuals (688 female) at 60-64y in the MRC National Survey of Health and
57 Development. Lumbar lordosis angle (L4 inferior endplate to T12 superior endplate) was
58 measured using the two-line Cobb method. In analyses adjusted for sex, height, lean and fat
59 mass, socioeconomic position and birthweight, later walking age was associated with greater
60 lordosis described by SSM1 (regression coefficient 0.023, 95%CI 0.000-0.047, $p=0.05$) and
61 direct angle measurement. Modest associations between walking age and less variation in
62 anterior-posterior vertebral size caudally (SSM6) were also observed (0.021, 95%CI -0.002-
63 0.044, $p=0.07$). Sex interactions showed that later walking was associated with larger relative
64 vertebral anterior-posterior dimensions in men (SSM3; -0.043, 95%CI -0.075-0.01, $p=0.01$)
65 but not women (0.018, 95%CI -0.0007-0.043, $p=0.17$). Similar associations were observed
66 between age at independent standing and SSMs but there was little evidence of association
67 between sitting age and spine shape. Unadjusted associations between walking age and SSMs
68 1 and 6 remained similar after adjustment for potential confounders and mediators. This
69 suggests that these associations may be explained by altered mechanical loading of the spine
70 during childhood growth, although other factors could contribute. Early life motor
71 development, particularly walking, may have a lasting effect on features of spine morphology
72 with clinical significance.

73 **Keywords:** Growth, mechano-adaptation, loading

74 **Introduction**

75 Infancy and early childhood represent key periods for the development of spine shape and
76 structure. Lordosis (indicated by the lumbosacral angle) increases from 20° to 70° in the first
77 five years of life ¹, followed by slower growth in both lordosis and thoracic kyphosis up to
78 adulthood ². In contrast, cervical lordosis increases until 9-10 years of age before decreasing
79 throughout adolescence ³. Vertebral height and width increase dramatically in the first two
80 years of life, after which time more modest growth continues until adulthood ⁴. These growth
81 patterns are highly dependent on vertebral location, with greater growth in lumbar than
82 thoracic and in turn cervical bodies ⁴ in line with the loading they experience. Due to these
83 increases in both vertebral size and bone mineral density, lumbar spine bone mass increases
84 fivefold between the ages of 1 to 36 months ⁵.

85 A key factor in the development of spine shape during this period is attainment of motor
86 milestones at 6-24 months of age. This development coincides with a large increase in
87 lordosis, and this angle is closely associated with stages of motor development such as
88 standing, walking and running ¹. The influence of early life motor development on spine
89 shape can also be examined through comparison with groups where attainment of motor
90 skills is impaired. Children with cerebral palsy display impaired growth of vertebral bodies,
91 with these deficits emerging after typical walking age at around 2 years ⁴. In children with
92 osteogenesis imperfecta, earlier attainment of independent sitting is associated with delayed
93 development of scoliosis ⁶. However, it is unknown whether associations between early life
94 motor development and spine shape persist into adulthood.

95 Development of spine shape involves simultaneous but discordant regional changes in
96 vertebral size and shape, as well as overall curvature ^{7;8}. Studies of spine shape have typically
97 described only a small number of these variables. Statistical shape modelling (SSM) can

98 provide an objective description of variation in these and other aspects of spine shape (such
99 as degree of variation in vertebral size within an individual's spine). SSM has been shown to
100 be more reliable and accurate than traditional measurements of spinal curvature ^{9; 10}.

101 Therefore, our primary aim was to examine whether early childhood motor development, as
102 indicated by age of attainment of independent walking is associated with spine shape in older
103 age using data from the MRC National Survey of Health and Development (NSHD), a British
104 birth cohort study. Walking age was selected as the motor milestone of primary interest
105 because of the large loads experienced during this movement ¹¹ and previous reports of strong
106 associations between walking age and bone health throughout life ¹²⁻¹⁴. Whilst spine shape
107 was our primary outcome, as a secondary aim we also examined associations between
108 walking age and osteoarthritis of the spine to assess whether there was any evidence that our
109 main findings have clinical consequences that are detectable in early old age. As age at
110 attainment of sitting and standing have also been associated with skeletal development ^{1; 6},
111 and are highly correlated with age at walking, associations between these exposures and spine
112 shape were also assessed as secondary analyses. It was hypothesised that the age at which
113 independent walking was attained would be associated with variation in spine shape features
114 in early old-age.

115 **Methods**

116 *Study Population*

117 The NSHD is a birth cohort study consisting of a socially-stratified sample of 5,362 singleton
118 births in 1 week in March 1946 in England, Scotland and Wales. These participants have
119 been prospectively followed regularly since birth¹⁵. Between 2006-2010, eligible participants
120 known to be alive and living in England, Scotland and Wales were invited for an assessment
121 at one of six clinical research facilities (CRF). Of 2856 individuals invited, 1690 attended a
122 CRF and 539 received a home visit from a research nurse. Ethical approval for this data
123 collection was obtained from the Central Manchester Research Ethics Committee
124 (07/H1008/245) and the Scottish A Research Ethics Committee (08/MRE00/12).

125 *Spine DXA images*

126 During the CRF assessment, images of the total body and spine were obtained using a QDR
127 4500 Discovery dual-energy X-ray absorptiometry (DXA) scanner (Hologic, Inc., Bedford,
128 MA). In five centres, scanners had rotating C-arms allowing participants to lie supine for all
129 scans, whilst one centre used a scanner with a fixed C-arm requiring participants to be
130 scanned in a lateral decubitus position. In both cases, participants were scanned with hips and
131 knees flexed, and with arms raised so as not to obscure the scanned region. Judith E Adams's
132 laboratory performed quantitative analysis of all scans and assessments for image quality. A
133 manufacturer-provided phantom was scanned daily prior to participant scanning; once a
134 month, these results were sent to the coordinating centre for scrutiny.

135 *Statistical shape modelling*

136 Of the 1690 participants who attended a CRF, 1601 had a spine DXA scan. 72 images were
137 excluded from analysis: in 41 images vertebral outlines could not be clearly determined, 23
138 had scanning artefacts, five did not include all vertebrae of interest, two included metalwork

139 and excessive axial rotation was observed in one image. This left 1529 images which were
140 used to build the SSM; this process has been described in detail previously ¹⁶. Briefly,
141 custom-made Shape software (University of Aberdeen) was used to create a template of 89
142 points including all vertebrae from the tenth thoracic vertebra (T10) to the superior endplate
143 of the fifth lumbar vertebrae. These eight vertebrae were chosen for analysis as they were
144 visible on all scans. Following an automatic search and placement of points, all images were
145 manually checked and where necessary points were adjusted. Mean intra- and inter-rater
146 repeatability for this technique is 1.4 and 2.2 pixels respectively ¹⁶, which represents a small
147 error considering an average spine image size of 1200 x 400 pixels and a typical vertebra size
148 of approximately 80 x 60 pixels. Procrustes transformation was used to translate, rotate and
149 scale the images to remove influences of size and alignment. Principal component analysis
150 was then performed to generate independent orthogonal modes of variation, describing in
151 descending order of percentage variation standardised to a mean of 0 and standard deviation
152 of 1. Eight modes (SM1 to SM8) were identified which each accounted for >1% spine shape
153 variation ranging from SM1 which accounted for 53.0% of variation to SM8 which accounted
154 for 1.2%; in total these eight modes accounted for 84.9% of the total variance ¹⁶. Lumbar
155 lordosis angle was measured using the two-line Cobb method ¹⁷ between the inferior endplate
156 of L4 and the superior endplate of T12. For each endplate we used the statistical shape model
157 point co-ordinates for the vertebral 'corners' to plot a line and calculate the slope of that line.
158 Using custom-written code in MATLAB (R2018a, The Mathworks, Natick, MA) the angle of
159 intersection of the two lines was calculated in degrees for each image in the dataset.

160 *Age at Onset of Independent Walking*

161 The age in months at which their child first walked unaided was recalled by participants'
162 mothers during an assessment at age 2 years.

163 *Covariates*

164 Potential confounders and mediators of the main associations between walking age and each
165 spine shape mode were selected *a priori* based on existing literature^{12; 16; 18}. The potential
166 confounders were birthweight, childhood socioeconomic position (SEP), adult SEP and
167 height, and the potential mediators were appendicular lean mass and appendicular fat mass.
168 Birthweight was extracted from medical records within a few days of birth, and
169 measurements to the nearest quarter-pound (113 g) were converted to kilograms. As
170 indicators of socioeconomic position (SEP), father's occupation at age 4 years (or at age 11
171 or 15 if missing at age 4) and own occupation at age 53 years (or if not available, the most
172 recent measure in adulthood) were both categorized into six groups (I [professional], II
173 [managerial and technical], IIINM [skilled non-manual], IIIM [skilled manual], IV [partly
174 skilled], and V [unskilled]) using the Registrar General's Social Classification¹⁹. During the
175 CRF visit, height was measured to the nearest mm and recorded in cm, and appendicular lean
176 and fat mass in kilograms were estimated from total body DXA scans.

177 *Statistical Analysis*

178 We include 1327 participants (688 women) in our models; of the 1529 participants with spine
179 shape mode data, 106 had missing data on age of independent walking and a further 96 had
180 missing data on covariates. Complete case analysis was undertaken using the R statistical
181 environment (version 3.2.2, www.r-project.org). Associations between age at onset of
182 independent walking and each spine shape mode were assessed using multiple linear
183 regression models. There was no evidence of deviation from linearity when quadratic terms
184 were included, so walking age was modelled as a continuous linear variable. Walking
185 age*sex interactions were examined given previous findings of sex-specific associations of
186 walking age with bone outcomes¹². Where sex interactions were identified ($P < 0.1$),
187 subsequent models were sex-stratified. Model 1 was adjusted for sex (unless sex-stratified)

188 and CRF location (as one CRF used a scanner with a fixed C-arm requiring participants to be
189 moved between scans). The impact of adjustment for each of the confounders and mediators
190 identified above was then examined in turn before all covariates were entered into a final
191 model (Model 2) simultaneously. Associations between walking age and lumbar lordosis
192 angle were assessed using the same model structures.

193 In addition to describing associations between walking age and individual mode scores, we
194 wanted to examine how overall spine shape described by these modes varied between earlier
195 and later walkers. Therefore, we combined mean mode scores for early walkers (defined as -
196 2SD below the mean walking age (i.e. 9.0 months)) and late walkers (defined as +2SD above
197 the mean walking age (i.e. 18.5 months)) for both women and men to generate mean spine
198 shapes.

199 *Sensitivity Analyses*

200 Whilst the prevalence of radiographic spine osteoarthritis in the NSHD cohort is low, we
201 investigated whether there were any associations between walking age and osteoarthritis of
202 the spine at age 60-64. DXA images were graded using a validated atlas scoring system²⁰,
203 with grades of 0-3 for each vertebra (T10-L4) summed to give a Total Lane Grade (TLG).
204 We also assessed associations between sitting (mean 6.5±1.4 months) and standing age (mean
205 11.4±2.1 months) obtained at the same maternal interview as walking age, and spine shape
206 modes using models described above.

207 **Results**

208 Characteristics of the participants in this study are detailed in Table 1 and spine shapes
209 described by each mode are presented in Supplementary Figure S-1. Scores for SM1, SM3
210 and SM8 were greater in women than men, whereas men had a higher score for SM6. Lumbar
211 lordosis angle was also greater in women than men.

212 Later age at onset of independent walking was weakly associated with greater SM1 scores in
213 Model 1 (regression coefficient 0.019, 95%CI -0.004 to 0.041), this association was
214 strengthened in fully-adjusted Model 2 (0.023, 95%CI 0.000-0.047). This suggests that
215 associations in Model 1 were obscured by negative confounding, although further analyses of
216 individual factors suggested that this was not attributable to any one single covariate (Table
217 2).

218 There was some evidence to suggest that later walking age was also weakly associated with
219 greater SM6 scores in Model 1 (0.021, 95%CI -0.002 to 0.043); this association was similar
220 in Model 2. Sex interactions were evident for SM3 in Model 1, with later walking age
221 modestly associated with lower scores in men and higher scores in women. In Model 2, the
222 interaction was stronger due to a strengthening of the negative association in males. There
223 was no evidence of associations between walking age and SM 2, 4, 5, 7 or 8.

224 When taking findings for SM1, 3 and 6 together, in later walkers these modes describe
225 greater lumbar and thoracic lordosis (SM1), and more uniform anterior-posterior vertebral
226 body diameter relative to vertebral height throughout the spine (SM6). Sex interactions in
227 SM3 indicated greater relative anterior-posterior vertebral size in late-walking men but not
228 women. In support of features described by associations with SM1, walking age was also
229 associated with greater lumbar angle corresponding to an increase in lordosis of 0.57° (95%
230 CI 0.36° to 0.78° , $P = 0.007$) for every 1 SD (around two months) increase in walking age in

231 Model 2. Mean spine shapes generated for early and late-walking men and women are shown
232 in Figure 1.

233 *Sensitivity Analyses*

234 Prevalence and severity of radiographic OA was low in this cohort; 301 individuals (23%)
235 had no evidence of degeneration (grade 0) at any vertebrae, and 898 individuals (68%) had
236 only mild degeneration (grade ≤ 1) at any vertebrae. No associations were observed between
237 walking age and TLG when the latter was modelled either as a continuous or dichotomous
238 variable (based on a TLG > 0 as cut-off) ($P > 0.4$ in both cases). Sitting age was weakly
239 positively associated with walking age ($r^2 = 0.18$, $P < 0.001$), and was weakly negatively
240 associated with spine shape mode 5 only (Supplementary Table 1, $P = 0.06$). There was a
241 strong positive association between standing age and walking age ($r^2 = 0.64$, $P < 0.001$).
242 Standing age was weakly positively associated with SM1 scores in Model 2 only (regression
243 coefficient 0.022, 95%CI -0.004 to 0.047), and with SM6 scores in both models. There was
244 evidence of sex interactions for SM3 with later standing age associated with lower scores in
245 men and higher scores in women, and for SM5 with later standing age associated with lower
246 scores in women only

247 **Discussion**

248 The aim of this study was to investigate associations between early life motor development
249 and components of spine shape described by statistical shape models in early old age. In
250 fully-adjusted models, later walking age was modestly associated with greater lordosis and
251 more even vertebral size along the spine, and with greater relative vertebral size in men but
252 not women. Similar associations were observed for later standing age but not for sitting age.

253 *Comparison with previous findings*

254 To our knowledge, this is the first study to investigate associations between early life motor
255 development and spine shape in adulthood. Previous studies have shown associations
256 between attainment of motor development milestones and lordosis in early childhood ¹.
257 Impaired or delayed motor development has previously been shown to be associated with
258 spine development. Children with cerebral palsy are at risk of developing excessive lordosis
259 of the lumbar spine ²¹, similar to observations of greater lordosis in late walkers in this study.
260 We have previously reported associations between walking age and spine area in males only
261 in this cohort ¹², which would initially seem to contradict findings of smaller vertebral size in
262 males in this study. However, as can be seen in Figure 1 and Supplementary Figure S-1 these
263 differences are subtle and unlikely to have a substantial influence on overall vertebral area.
264 More importantly, images are scaled prior to generation of shape modes thereby removing
265 differences in overall size. Greater vertebral size in SM6 therefore represents the relative
266 anterior-posterior to cranial-caudal proportions of vertebral bodies, which could result from
267 narrower and/or taller vertebrae. As walking age is positively associated with height in this
268 cohort, greater vertebral height could explain these apparently conflicting associations.
269 Similar associations to those observed between walking age and spine shape were observed
270 for standing age, which was highly correlated with walking age, but there was little evidence

271 of associations between sitting age and spine shape. This is similar to findings of previous
272 studies in younger children, where walking age but not crawling or standing age was
273 associated with tibia mass and geometry ¹⁴.

274 *Possible explanation of findings*

275 Walking is associated with lumbosacral loads of around 1.6 times bodyweight, which is 60%
276 greater than those achieved during standing ¹¹. Therefore, attainment of independent walking
277 exposes the spine to large increases in loading at a time of rapid development. The smaller
278 loads associated with static activities may explain the lack of association between sitting age
279 and spine shape. The importance of larger locomotory loads for spine health is supported by
280 the large bone losses associated with loss of ambulation such as in long-term spaceflight ²².
281 Initially, vertebral size is similar throughout the spine ²³ but differences between lumbar and
282 thoracic vertebrae emerge around onset of walking ⁴. Reduced variation in relative vertebral
283 size in late walkers may therefore reflect reduced loading variation throughout the spine
284 during this period. Greater back extensor muscle size has previously been associated with
285 greater lumbar lordosis ²⁴, but there was little evidence of associations between lean mass and
286 spine shape modes in this study, and adjustment for lean mass did not attenuate association
287 between walking age and spine shape modes.

288 *Significance and implications*

289 Greater lumbar lordosis, described by SM1 and the lumbar angle, identified in late walkers in
290 the current study have been shown to be associated with spondylolysis and isthmic
291 spondylolisthesis in other studies ²⁵. A recent study also found that smaller relative anterior-
292 posterior size, observed in late-walking women in this study, was also associated with
293 spondylolysis ²⁶. A number of clinical groups with delayed ambulation including Down
294 syndrome ²⁷, osteogenesis imperfecta ²⁸ and dyskinetic cerebral palsy ²⁹ have increased risk

295 of spondylolysis and/or isthmic spondylolisthesis, therefore motor deficits in early life may
296 contribute to these problems. If delayed motor development is shown to influence
297 spondylolysis risk in late walkers, there may be interventional opportunities to minimise
298 these effects. Parent-led walking training can lead to earlier walking onset in the general
299 population³⁰ and clinical cohorts such as children with Down syndrome³¹. In children with
300 myelomeningocele, these interventions appear effective in reducing deficits in bone mass³².
301 Whilst the effects of walking training on joint shape are unknown, future interventional
302 studies investigating these effects could establish motor development as a modifiable factor
303 influencing lifelong spine health. There is conflicting evidence as to whether lumbar lordosis
304 is associated with other types of lower back pain and osteoarthritis²⁵, but these associations
305 were not found in the cohort examined in this study³³. We found no evidence of associations
306 between walking age and radiographic OA, although the incidence of OA was very low in
307 this cohort. In addition, to our knowledge there have been no previous investigations of
308 associations between the reduced curvature in the lower thoracic region observed in late
309 walkers in this study and clinical outcomes. Previous observations of lower bone mass in
310 male late walkers in this cohort¹² suggest an increased risk of fracture, but it is not clear
311 whether spine shape features identified in the current study could influence this risk. Future
312 studies examining associations between motor development and spine pathologies could help
313 reveal the clinical consequences of delayed attainment of motor milestones.

314 *Strengths and weaknesses*

315 The cohort examined in this study is broadly representative of the British-born population of
316 the same age³⁴, which allows us to generalise these results to this population. In addition, the
317 cohort have been followed for over six decades since birth, allowing us to adjust for potential
318 confounders which were obtained prospectively. Most importantly, details of early life motor
319 development were obtained six decades previously by maternal recall at two years, which has

320 been shown to be highly reliable ^{35;36}. Previous studies have shown that associations between
321 early life motor development and adolescent bone outcomes are mediated by childhood
322 physical activity ¹². Due to limited information on physical activity in early life we were
323 unable to explore this potential mediating pathway, although walking age is not associated
324 with adult physical activity in this cohort ³⁷. As an observational study we cannot attribute
325 causality, and residual confounding and bias due to drop out and missing data in this cohort ³⁸
326 may have influenced the results. Caution is required in interpreting these findings and
327 considering their implications, because evidence suggests that some of the associations we
328 have observed in this study are modest. In addition, the overall shape differences between
329 early and late walkers described by statistical shape models are quite subtle. However, even
330 these small differences (0.2-0.4SD) are similar to those identified between individuals with
331 and without long-term back pain in the same cohort ³³ suggesting that they may prove to be
332 clinically relevant with increasing age. Spine images were taken with participants in a supine
333 position with hips and knees flexed which would result in differences in spine morphology
334 compared to standing. However, we have shown previously that inter-individual variation in
335 spine shape is preserved throughout a full range of extension to flexion and in a range of
336 postures ^{39;40} therefore the current results likely reflect spine shape variation independent of
337 position. In addition, we could only measure down to inferior endplate of vertebra L4 as the
338 inferior endplate of vertebra L5 was not consistently visible, so measures of lumbar angle
339 from T12 to L4 are surrogate measures of the full lumbar lordosis angle.

340 *Conclusions*

341 Later age at onset of independent walking in early childhood is modestly associated with
342 features of spine shape in early old age, namely with greater lordosis and less variation in
343 vertebral size along the spine, and relative vertebral size is greater in male later walkers but
344 not females. These associations were also observed with standing but not sitting age and were

345 independent of a number of potential confounders and mediators, which suggests that they
346 could result from altered mechanical loading during a key phase of growth in early
347 childhood. Clinically, greater lumbar lordosis and smaller vertebral size are associated with
348 spondylolysis and isthmic spondylolisthesis and a number of clinical populations with
349 delayed motor development have greater incidence of these conditions. Early life motor
350 development, in particular walking onset age, appears to have a small persisting effect on
351 features of spine morphology with clinical relevance throughout life. Given that training
352 interventions can promote earlier walking onset, age at onset of independent walking may
353 represent a novel modifiable factor to improve spine development particularly in populations
354 in which delayed motor development and spine problems are common.

355

356 3634 Words

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360

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476

477 Table 1. Characteristics of the MRC National Survey of Health and Development stratified
 478 by sex (sample restricted to those with complete spine shape mode data and covariates).

Variable		Women (n=688)		Men (n=639)		Sex difference P-value
		Mean	SD	Mean	SD	
Walking Age (months)		13.7	2.4	13.7	2.3	0.6
Birthweight (kg)		3.39	0.63	3.45	0.57	0.05
		<i>n</i>	%	<i>n</i>	%	
Father's Occupational Class (age 4y)	I	51	7.4%	58	9.1%	0.72
	II	158	23.0%	141	22.1%	
	IIINM	130	18.9%	125	19.6%	
	IIIM	195	28.3%	184	28.8%	
	IV	122	17.7%	97	15.2%	
	V	32	4.7%	34	5.3%	
Own Occupational Class (age 53y)	I	14	2.0%	86	13.5%	<0.01
	II	293	42.6%	303	47.4%	
	IIINM	246	35.8%	71	11.1%	
	IIIM	39	5.7%	136	21.3%	
	IV	73	10.6%	35	5.5%	
	V	23	3.3%	8	1.3%	
Musculoskeletal assessments at 60-64y						
		Mean	SD	Mean	SD	
Age at time of assessment (y)		63.2	1.1	63.1	1.2	0.09
Height (m)		1.62	0.06	1.75	0.06	<0.01
Weight (kg)		71.4	12.3	84.9	12.6	<0.01
Appendicular Lean Mass (kg)		16.1	2.4	24.6	3.3	<0.01
Appendicular Fat Mass (kg)		14.3	4.1	10.0	2.8	<0.01
Lumbar lordosis angle (°)		13.1	7.7	11.5	7.2	<0.01
Spine Shape Mode (SM) Scores	SM1	0.07	1.02	-0.05	0.96	0.03
	SM2	-0.03	0.99	0	1	0.62
	SM3	0.47	0.78	-0.49	0.98	<0.01
	SM4	-0.05	1.02	0.03	0.98	0.12
	SM5	-0.04	0.97	0.05	1	0.1
	SM6	-0.18	0.98	0.19	0.96	<0.01
	SM7	-0.01	0.96	0.05	1.03	0.28
	SM8	0.23	0.92	-0.27	1	<0.01

479 Table 2. Associations between age at onset of independent walking and spine shape mode
 480 outcomes in the MRC National Survey of Health and Development. Regression coefficients
 481 are the difference in mean SM score per 1 month increase in walking age. Where sex
 482 interactions were evident (P for interaction < 0.1), sex-specific associations are presented.

Mode	Group	Model	Regression coefficient	95% CI		P	Sex Interaction P
SM1	Combined	1	0.019	-0.004	0.041	0.1	0.28
		2	0.023	0.000	0.047	0.05	0.36
SM2	Combined	1	-0.002	-0.025	0.021	0.88	0.76
		2	-0.014	-0.037	0.010	0.25	0.79
SM3	Men	1	-0.024	-0.056	0.008	0.15	0.03
	Women		0.021	-0.004	0.046	0.09	
	Men	2	-0.043	-0.075	-0.010	0.01	<0.01
	Women		0.018	-0.007	0.043	0.17	
SM4	Combined	1	-0.013	-0.037	0.010	0.25	0.14
		2	-0.006	-0.030	0.017	0.6	0.14
SM5	Combined	1	-0.011	-0.034	0.012	0.35	0.34
		2	-0.017	-0.040	0.007	0.17	0.45
SM6	Combined	1	0.021	-0.002	0.043	0.07	0.94
		2	0.021	-0.002	0.044	0.07	0.91
SM7	Combined	1	0.007	-0.016	0.030	0.54	0.56
		2	0.006	-0.018	0.030	0.63	0.39
SM8	Combined	1	0.002	-0.020	0.024	0.84	0.19
		2	0.010	-0.012	0.033	0.36	0.24

483

484 Footnote: Model 1 adjusted for Sex (if men and women are combined) and Clinic, Model 2:
 485 Model 1 + Birthweight + Father's occupational Class + Adult Occupational Class + Height +
 486 Appendicular Fat Mass + Appendicular Lean Mass. Only results from basic and fully-adjusted
 487 models are presented for brevity. When each set of covariates were adjusted for in turn there
 488 was no evidence that any one specific set of factors was responsible for the attenuations
 489 observed between the models shown here.

490 Figure 1. Mean spine shapes described by statistical shape models in early (-2SD of the mean
491 age) and late-walking (+2SD of the mean age) men and women.

492 Footnote: The mean age of walking in this cohort was 13.7 ± 2.3 months with no sex
493 difference. Therefore, early and late walking as described above corresponded to walking at
494 9.0 months and walking at 18.5 months respectively.