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Nicholson, VP, Spathis, JG, Hogarth, LW, Connick, MJ, Beckman, EM, Tweedy, SM, Payton, CJ and Burkett, BJ (2018) Establishing the reliability of a novel battery of range of motion tests to enable evidence-based classification in Para Swimming. *Physical Therapy in Sport*, 32. pp. 34-41. ISSN 1466-853X

DOI: <https://doi.org/10.1016/j.ptsp.2018.04.021>

Publisher: Elsevier

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**ESTABLISHING THE RELIABILITY OF A NOVEL BATTERY OF RANGE OF MOTION
TESTS TO ENABLE EVIDENCE-BASED CLASSIFICATION IN PARA SWIMMING**

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This research was supported by the International Paralympic Committee (IPC), UK Sport, and Exercise & Sports Science Australia (Applied Sports Science Research Grant). Mark Connick, Emma Beckman and Sean Tweedy are members of the IPC Classification Research and Development Centre (Physical Impairments), which is supported by the International Paralympic Committee. The authors would like to acknowledge Jayden Lowrie, Samantha Yardy-Phelan and Ana Maia for their assistance in data collection.

1 **Abstract**

2 Objectives: To evaluate the reliability of swimming-specific range of movement tests developed in
3 order to permit evidenced-based classification in the sport of para swimming.

4 Design: Test-retest intra- and inter-examiner reliability.

5 Setting: International Swimming training camps and university exercise science departments.

6 Participants: 42 non-disabled participants (mean age 23.2 years) and 24 Para swimmers (mean age
7 28.5 years).

8 Main Outcome Measures: Intra- and inter-examiner reliability of a battery of novel active range of
9 motion tests.

10 Results: Good to excellent intra-examiner reliability was found for the majority (32/34) of tests in
11 non-disabled participants (ICC = 0.85-0.98). SEM values ranged from 1.18° to 6.11°. Similarly,
12 good to excellent inter-examiner reliability was found for the majority (35/42) of tests in non-
13 disabled participants (ICC = 0.85-0.98). SEM values range from 0.73° to 6.52°. Para swimmers
14 exhibited significantly reduced range of motion compared to non-disabled participants.

15 Conclusions: The large majority of ROM tests included in this novel battery were reliable both
16 within and between examiners in non-disabled participants. The tests were found to differentiate
17 between non-disabled participants and Para swimmers with hypertonia or impaired muscle power.

18

19 **Key words:**

20 Swimming; Shoulder; Hip; Inclinometer

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INTRODUCTION

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Paralympic classification systems aim to promote participation in sport by people with disabilities by minimizing the impact impairment has on the outcome of competition (Tweedy & Vanlandewijck, 2011). Classification systems which achieve this aim will ensure that successful athletes are not simply those with the least impairment, but will be those that have the most advantageous combination of physiological and/or psychological attributes and who have trained them to best effect (Tweedy & Vanlandewijck, 2011). In 2007, the IPC Classification Code mandated the development of evidence-based systems of classification in Paralympic sport which are informed by scientific research (IPC, 2007).

The Paralympic games are the largest organized sporting event for athletes with disabilities with 164 participating countries and more than 1.8 million tickets sold at the 2016 Rio Paralympic Games (IPC, 2016). In Para Swimming, there are eight physical impairments comprising; impaired muscle strength, impaired passive range of movement (ROM), limb deficiency, leg length difference, short stature, hypertonia, ataxia, and athetosis (IPC, 2007). Eligible swimmers compete across ten classes in freestyle, backstroke and butterfly events (S1-S10) and nine classes in breaststroke events (SB1-SB9). The current classification process involves two-steps: 1) evaluation of impairment via a bench test (Dummer, 1999) and 2) a technical assessment known as a water test. The bench test involves evaluation of joint range of motion, which may be critical to determining an athlete's class in Para swimming. Impaired ROM is defined as a reduction in one or more joints which is reduced permanently (IPC, 2007). Impaired ROM from health conditions such as cerebral palsy, resulting in spasticity or contracture, for example are currently evaluated using a passive joint-by-joint assessment conducted by a trained classifier using a goniometer which is then scored against a passive functional ROM on a zero to five scale (IPC, 2017). The water test involves allocation of points based on an athlete's ability to perform key water skills specific to

1 swimming such as a dive start and push-off when turning. The classifier then totals the points
2 obtained from the bench test and the water test using established criteria and expert opinion to
3 determine a class (IPC, 2017).

4
5 For classification, these measures of impaired ROM in the bench test have advantages in that they
6 use widely utilized methods known to clinicians and the equipment is inexpensive and available
7 world-wide. However, there are several limitations of these measures, which make them unsuitable
8 methods of ROM assessment for classification. Firstly, the current system utilizes a ratio scaled
9 measure with a goniometer (Tweedy & Vanlandewijck, 2011) but then converts the outcome to a
10 point scale (zero to five) based on relative range of motion rather than allocating absolute values.
11 As such, an athlete that scores four points on a ROM measure does not necessarily have twice the
12 ROM as someone that scores two points. Weak relationships have been found between non-ratio
13 scale measures currently used in classification and sports performance (Beckman, Connick, &
14 Tweedy, 2016). Secondly, ROM is currently assessed using passive ROM techniques, where the
15 classifier moves the athlete's joints through a range applying external forces to the body, which has
16 questionable repeatability compared to active ROM techniques (Boon & Smith, 2000; Cools, et al.,
17 2014; De Winter, et al., 2004; Muir, Corea, & Beaupre, 2010). Thirdly, the reliability of the
18 majority of ROM tests currently included in the classification system are not known or their
19 reliability is difficult to determine due to significant variability in the positioning of the participant
20 and the equipment selected (i.e. inclinometer, goniometer, visual assessment or a combination) (van
21 de Pol, van Trijffel, & Lucas, 2010). Fourthly, ROM is assessed using a joint-by-joint method
22 which is not parsimonious, is time intensive and little evidence exists to show the impact of
23 individual joint ROM on swimming performance. For example, only weak correlations exist
24 between current ROM classification measures and swimming propulsion and joint kinematics
25 (Evershed, Frazer, Mellifont, & Burkett, 2012). Additionally, measures of impairment should only

1 assess body structures that will impact on performance in body positions relevant to sports
2 performance (Tweedy & Vanlandewijck, 2011) and that can be achieved by all eligible athletes
3 regardless of impairment type or severity. The current ROM tests do not necessarily assess ROM in
4 positions relevant to swimming, and neglect certain swimming specific positions such as streamline
5 and prone shoulder flexion. These limitations threaten the validity of the classification system and
6 can result in failure to delineate performance between some classes and disadvantaging athletes
7 with certain types of physical impairment within classes (Evershed, et al., 2012; Howe & Jones,
8 2006; Oh, Burkett, Osborough, Formosa, & Payton, 2013).

9

10 Given the limitations of current passive ROM tests and in order to permit evidence-based methods
11 of classification, the development of a battery of novel ROM measures for swimming is required
12 (Tweedy, Beckman, & Connick, 2014). The characteristics of the battery are required to comply
13 with the IPC Position Stand on Classification which states that tests of impairment be objective,
14 reliable, precise, ratio-scaled and valid (Tweedy, et al., 2014; Tweedy & Vanlandewijck, 2011).
15 Additionally, the tests of impairment should be impairment specific, as resistant to training as
16 possible, comprehensive by addressing movement relevant to the sport, and parsimonious.

17

18 The aim of the study was to enable evidence-based classification in Para swimming by establishing
19 the reliability and preliminary normative values for a battery of swimming-specific range of motion
20 tests by: 1) evaluating the intra-examiner and inter-examiner reliability of each novel ROM measure
21 in non-disabled participants; 2) providing preliminary normative values for a novel ROM
22 assessment battery in non-disabled participants and a group of trained Para swimmers; and 3)
23 determining if differences exist for the novel ROM battery outcomes between non-disabled
24 participants and Para swimmers.

METHODS

Participants

Two groups of participants were tested: Group 1 comprised 42 (20 males, 22 females) non-disabled physically active, injury free individuals engaging in at least 90 minutes of moderate physical activity per week. These participants were recruited from two Australian Universities. Group 2 comprised 24 (17 males, 7 females) elite Para swimmers who were nationally or internationally classified (classes S1-S8) and were undertaking planned training regimes and competing at national or international level. Group 2 included athletes with spinal cord injury (SCI), polio, cerebral palsy (CP) or acquired brain injury (ABI) - conditions that can result in one of, or a combination of impaired ROM, impaired strength or impaired coordination. These Para swimmers were categorized into two subgroups: those with hypertonia associated with CP and ABI (n=11, 9 males, 2 females); and those with impaired muscle power resulting from SCI or polio (n=13, 8 males, 5 females). While both subgroups may demonstrate some impairment in ROM, each subgroup has different ROM patterns due to the nature of their health condition. Athletes were from England, Spain, Italy and Czech Republic.

Study Design and Procedures

Data collection was conducted by three PhD trained staff with professional qualifications in the movement sciences with experience working with elite athletes with disabilities. All reliability testing was undertaken within University Exercise Science facilities. Assessment of Para swimmers was undertaken at various training facilities within Europe. All participants provided written informed consent and the study was approved by the Human Research Ethics Committees of the lead author's institution.

1 Non-disabled participants and Para swimmers completed a baseline questionnaire regarding
2 demographics, training (number and types of sessions per week) and injury history.
3 Anthropometric measures (standing height (m), body mass (kg), body mass index (BMI)) were also
4 assessed prior to ROM assessment. Range of motion (ROM) testing was conducted with an Acumar
5 Digital Inclinometer (Lafayette Instrument Co. Lafayette, IN), which was zeroed and aligned with
6 the appropriate reference point (horizontal or vertical) before each test. A universal goniometer
7 (Baseline Evaluation Instruments, White Plains, NY) was also used to compare reliability and ease
8 of administration for elbow flexion and extension (inter-examiner study). Trunk functional reach
9 measures were obtained with a supported fixed tape measure.

10 Measures from the 42 non-disabled participants were used to establish preliminary
11 normative values. Fifteen of these non-disabled participants also took part in intra-examiner
12 reliability testing while a further 16 took part in inter-examiner testing. Para swimmers completed
13 the ROM test battery on one occasion to provide preliminary normative data for the ROM tests and
14 to compare whether differences existed between subgroups of Para swimmers and between Para
15 swimmers and non-disabled participants. Intra-examiner reliability: fifteen non-disabled
16 participants completed two, one-hour testing sessions. Participants were tested by a single examiner
17 on two occasions with at least one day between testing sessions. Two trials of each test were
18 conducted on each participant following a practice trial, and the average of the results used for
19 analysis.

20 Inter-examiner reliability testing: sixteen non-disabled participants completed a single two-
21 hour testing session and were tested independently by two examiners for all ROM tests within a
22 single session. Two trials of each test were conducted on each participant following a practice trial,
23 and the average of the results used for analysis. Testing followed the same standardized order for
24 each participant for both the intra- and inter-examiner reliability protocols.

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3 Tests of range of motion (ROM)

4 Active range of motion was assessed via a battery of 10 tests designed to measure shoulder, elbow,
5 hip, knee, ankle and trunk motion relevant to S-class swimming events (freestyle, backstroke and
6 butterfly strokes). These 10 tests produced over 30 measures as some tests assessed multiple joints.
7 All measures were demonstrated by the examiner before being performed by the participant. The
8 following landmarks were located and marked with a semi-permanent pen prior to ROM assessment
9 to provide consistency of inclinometer placement: lateral aspect of acromion process; lateral
10 epicondyle; ulna and radial styloid processes; greater trochanter; lateral knee joint line; tibial
11 tuberosity; lateral malleolus; anterior aspect of talus; dorsal aspect of 2nd metatarsophalangeal
12 (MTP) joint. Mid-points between adjacent landmarks were measured and marked, then used to
13 place the digital inclinometer. For example, the mid-point between the lateral aspect of the
14 acromion process and lateral epicondyle was used as the upper arm landmark to measure shoulder
15 abduction. Detailed descriptions for all tests can be found in supplementary material
16 (supplementary Table 1).

- 17 i) Bilateral Shoulder flexion (streamline)
18 ii) Bilateral Shoulder abduction (streamline)
19 iii) Elbow flexion and extension
20 iv) Lower-limb streamline (hip, knee and ankle extension)
21 v) Hip and knee flexion
22 vi) Shoulder internal and external rotation
23 vii) Prone shoulder extension (in elbow flexion and extension)

- 1 viii) Prone shoulder horizontal abduction
- 2 ix) Prone shoulder flexion
- 3 x) Trunk functional reach (forward, backward, sideways)

4

5 Data analysis

6 Data were analyzed using IBM SPSS 22 for Windows. All variables were examined for normality
7 using the Shapiro-Wilk test. A two-way mixed model intra-class coefficient ($ICC_{3,2}$) was used to
8 determine reliability between session one and two for intra-examiner reliability, and between
9 examiners for inter-examiner reliability (Shrout & Fleiss, 1979) for non-disabled participants.
10 Absolute agreement between sessions for intra-examiner and between examiners for inter-examiner
11 reliability was based on the mean of two values from each session and examiner, respectively. Good
12 to excellent reliability was defined a priori as an $ICC > 0.75$, moderate reliability defined as an ICC
13 $0.5-0.75$ and poor reliability defined as an $ICC < 0.5$ (Portney & Watkins, 2009). ICC values may
14 be high despite poor trial to trial consistency if the inter-subject variability is too high (Weir, 2005),
15 to negate this issue, the standard error of measurement (SEM) [$SEM = \text{Average Standard deviation}$
16 $\times \sqrt{(1 - ICC)}$] was also calculated as this is not affected by inter-subject variability.

17 Paired-samples T-tests were conducted to identify any differences between testing sessions
18 or between examiners. One-way ANOVA was used to identify differences in ROM between non-
19 disabled participants, Para swimmers with hypertonia and Para swimmers with impaired muscle
20 power. Post-hoc comparisons using Tukey HSD were applied when a difference between means
21 was identified within the ANOVA. Significance was set at $\alpha < 0.05$.

22

23

RESULTS

1 Intra-examiner reliability

2 Fifteen non-disabled participants aged 21.9 (\pm 3.4) years took part in the intra-examiner reliability
3 study. Each participant was tested by the same examiner with each test session separated by 4.1 (\pm
4 2.7) days. The majority of tests produced good to excellent (>0.75) ICC absolute agreement values
5 (Table 2). There were three exceptions where moderate reliability values were obtained: bilateral
6 shoulder abduction ($ICC_{3,2} = 0.73$), functional reach forwards ($ICC_{3,2} = 0.66$) and functional reach
7 right ($ICC_{3,2} = 0.68$). SEM values ranged from 1.18° to 6.11°.

8 There were no significant differences between sessions for any measures except elbow extension
9 left ($t = 2.32$, $p = 0.04$) with goniometer, lower-limb streamline left ankle angle ($t = 3.93$, $p < 0.01$),
10 and knee flexion left with goniometer ($t = -2.22$, $p = 0.04$) (Table 2).

11 Inter-examiner reliability

12 For the inter-examiner reliability study, 16 non-disabled participants aged 25.1 (\pm 5.1) years took
13 part in the study. All tests produced good to excellent (>0.75) ICC absolute agreement values
14 (Table 3) except for six measures that produced moderate reliability: elbow extension right with
15 inclinometer ($ICC_{3,2} = 0.75$); right elbow flexion with goniometer ($ICC_{3,2} = 0.67$) and right elbow
16 extension ($ICC_{3,2} = 0.73$) with goniometer; knee flexion right with goniometer ($ICC_{3,2} = 0.72$),
17 functional reach forwards ($ICC_{3,2} = 0.73$) and right ($ICC_{3,2} = 0.62$) together with one measure that
18 produced poor reliability: knee flexion left with goniometer ($ICC_{3,2} = 0.21$). SEM values ranged
19 from 0.73° to 6.52°.

20 There were significant differences between examiners for right elbow flexion ($t = 2.41$, $p = 0.03$)
21 and extension ($t = -2.88$, $p = 0.01$) with goniometer, left elbow flexion with inclinometer ($t = -3.96$,
22 $p < 0.01$) and goniometer ($t = 5.42$, $p < 0.01$), hip flexion left ($t = 2.69$, $p = 0.02$), knee flexion left

1 with goniometer ($t = -2.25$, $p = 0.04$), shoulder internal rotation left ($t = -3.10$, $p = <0.01$) and right
2 ($t = -2.71$, $p = 0.02$), (Table 3).

3 Preliminary normative values

4 There were significant differences between non-disabled participants and Para swimmers for the
5 majority of ROM tests (Table 4). Significant differences were also found between Para swimmers
6 with hypertonia and Para swimmers with impaired muscle power for certain measures at the trunk,
7 hip and knee (Table 4). Participant characteristics are presented in Table 1 and preliminary
8 normative values for each group are presented in Table 4.

9

10 DISCUSSION

11 The aim of this research was to enable evidence-based classification in Para swimming by
12 establishing the reliability and normative values for a battery of swimming-specific range of motion
13 (ROM) tests for swimmers. The results presented herein demonstrate that the majority of active
14 ROM assessments were reliable in non-disabled participants, and Para swimmers had significantly
15 less ROM than non-disabled participants. This finding addresses the key guidelines for the
16 international classification system, that is the measures of impairment for the purposes of
17 classification should be ratio scaled, reliable, precise and comprehensive by addressing movement
18 relevant to the sport (Tweedy & Vanlandewijck, 2011).

19 The key finding of this study is that the majority of ROM assessments used in this novel test battery
20 showed good to excellent levels of reliability in non-disabled participants. Establishing that the
21 measures are reliable within non-disabled participants is an essential step towards developing
22 evidence-based classification systems (Beckman & Tweedy, 2009). One of the important

1 differences between this novel test battery and the ROM assessments currently employed for Para
2 swimming classification is that this test battery assessed active ROM while the Para swimming
3 classification tests measure passive ROM. Active range of motion measurements are deemed to be
4 more reliable than passive measures, particularly in the shoulder (Boon & Smith, 2000; Cools, et
5 al., 2014; De Winter, et al., 2004; Muir, et al., 2010) which is of particular interest in Para
6 swimmers. When comparing our results to previous ROM reliability studies only a few measures
7 can be accurately scrutinized, as although some of the tests within this battery are used routinely
8 within swimming screenings and clinical assessments (Blanch, 2004), there is a paucity of literature
9 examining their reliability. Shoulder internal rotation and external rotation are two exceptions as
10 they are measures that have received repeated attention within the literature (Cools, et al., 2014;
11 Furness, Johnstone, Hing, Abbott, & Climstein, 2015; Riemann, Witt, & Davies, 2011; Walker, et
12 al., 2016). The intra-examiner values in this study (>0.80) for both internal and external rotation
13 were superior to some (Awan, Smith, & Boon, 2002; Walker, et al., 2016) but slightly lower than
14 others that have reported ICC values of greater than 0.9 (Cools, et al., 2014; Furness, et al., 2015)
15 using an inclinometer. The good to excellent reliability values found for inter-examiner assessment
16 are similar to previous studies that have also found good to excellent reliability values both in
17 swimmers (Riemann, et al., 2011; Walker, et al., 2016) and non-swimmers (Cools, et al., 2014;
18 Furness, et al., 2015). The generally low levels of SEM in this study indicate consistency across
19 testing sessions and between examiners for this test battery and compare favorably to previous
20 reliability studies that have reported SEM values of $2-5^{\circ}$ for active shoulder movements (Kolber,
21 Vega Jr, Widmayer, & Cheng, 2011; Walker, et al., 2016).

22 The ability to maintain optimal lower limb and trunk positions is important for swim performance
23 (Chatard, Lavoie, Bourgoin, & Lacour, 1990; Daly, Malone, Smith, Vanlandewijck, & Steadward,
24 2001; Zamparo, Gatta, Pendergast, & Capelli, 2009) but there is limited literature assessing the

1 reliability of lower limb measures in swimmers or young athletes as the majority of lower limb
2 reliability studies have been conducted in patient populations (van Trijffel, van de Pol, Oostendorp,
3 & Lucas, 2010). All lower limb tests in this study that were measured with an inclinometer
4 produced good to excellent levels of reliability. The lower limb reliability values and SEMs
5 established in our study for active ROM are superior to the majority of lower limb passive ROM
6 measures previously published (Currier, et al., 2007; van Trijffel, et al., 2010). For example, our
7 results for lower limb streamline ankle plantar flexion achieved excellent ICC values which is in
8 contrast to previous studies assessing plantar flexion that have reported poor to moderate levels of
9 inter-examiner reliability when assessed either actively (Youdas, Bogard, & Suman, 1993) or
10 passively (Elveru, Rothstein, & Lamb, 1988) with a goniometer. The superior results in our study
11 are likely due to the use of an inclinometer rather than a goniometer.

12 The choice of measuring instrument is an important consideration in ROM assessment and
13 consequently classification. The majority of tests that did not achieve good to excellent reliability in
14 this test battery were measured using a goniometer. Some of these measures such as knee flexion
15 and elbow flexion, were more reliable when obtained with an inclinometer, suggesting that the
16 inclinometer be the preferred method of measuring these movements, which is in contrast to current
17 Para swimming protocols that still use goniometers for ROM measures (IPC, 2017). Only one
18 measure across the test battery, left knee flexion with goniometer, achieved a poor level of
19 reliability (Portney & Watkins, 2009), suggesting that it may not be suitable for classification
20 purposes. The other tests that did not consistently achieve good to excellent reliability were
21 functional reach forwards and sideways. The reduced reliability in these trunk related measures was
22 most likely due to small variations in participants' sitting posture and difficulty maintaining the end
23 position long enough to obtain an accurate measurement. Despite these limited reliability concerns,
24 the tests were easily administered in non-disabled participants without the need for expensive

1 equipment – a requirement for any potential classification battery as the tests should facilitate
2 international dissemination and implementation (Tweedy & Vanlandewijck, 2011).

3 While the results indicate that the majority of tests used in this novel ROM battery are reliable,
4 classification methods need to be comprehensive by addressing movement relevant to the sport
5 (Tweedy & Vanlandewijck, 2011). The current classification system assesses passive shoulder
6 extension (in elbow extension) in prone but it does not assess active shoulder flexion or horizontal
7 abduction range of motion in prone. The battery of tests used in this study incorporated two
8 measures (tests vii) of shoulder extension (in both elbow flexion and extension) together with
9 horizontal abduction (test viii) as these tests replicate the arm positions during the recovery phase of
10 freestyle (Pink, Perry, Browne, Scovazzo, & Kerrigan, 1991). Prone shoulder flexion was also
11 incorporated (test ix) to replicate the entry and early pull phases of freestyle (Payton, Bartlett,
12 Baltzopoulos, & Coombs, 1999; Pink, et al., 1991). This unilateral shoulder flexion assessment is
13 distinct from the bilateral streamline position assessed in sitting (test i), as a swimmer's upper limb
14 streamline position is limited by the least mobile shoulder, but a swimmer's hand entry position or
15 early pull position can potentially vary substantially between sides (Evershed, et al., 2012). It is
16 therefore important that the ROM of both sides are captured independently otherwise an athlete
17 with a relatively poor streamline position due to limitations on one side will have an erroneous
18 representation of their actual ability to propel themselves with their less impaired side. Another
19 important addition to this test battery was lower limb streamline (test iv) which assesses ankle
20 plantar flexion with the knee and hip extended. The current system only assesses plantar flexion in
21 sitting so it does not capture the movement relevant to swimming where the ability to plantar flex
22 the ankle is important for maintaining a streamline position and kicking (Hull, 1990).

23

1 The current study has also established preliminary normative values for a new ROM test battery
2 designed for Para swimmers. Participants comprised athletes with health conditions including spinal
3 cord injury, cerebral palsy and acquired brain injury, which can result in impaired ROM, impaired
4 strength, impaired coordination, or a combination of these impairments. Athletes with disabilities
5 had significantly less ROM than non-disabled participants in the majority of ROM tests (Table 4).
6 These results indicate that divergent validity is evident within this test battery. That is, we would
7 expect people with impaired ROM to have lower scores than non-disabled people. Further analysis
8 indicated a difference within the group of athletes with disabilities. When comparing those with
9 either predominately impaired ROM associated with hypertonia (resulting from cerebral palsy and
10 acquired brain injury) and those with impaired muscle power (resulting primarily from spinal cord
11 injury) there were differences in ROM at the trunk, hip and knee. These differences are not
12 surprising given that all athletes with impaired muscle power had lesions that would limit their
13 ability to actively move or control their trunk and lower limbs. This outcome implies some degree
14 of discriminant ability within the test battery, but it should be noted that despite finding some
15 differences in the pattern of ROM between subgroups of athletes, the purpose of Paralympic
16 classification is to identify and measure impairment, rather than classify merely based on a medical
17 diagnosis (Tweedy & Vanlandewijck, 2011). Further research is needed to assess how impairments
18 in ROM impact swimming performance.

19 The final feature of this study was that the majority of assessments in the new test battery were
20 measured in a group of 24 Para swimmers. The study identified that the new test procedures are
21 feasible within a sample of athletes with disabilities – including those with severe impairments. For
22 example, two participants with impaired muscle power who compete in class S1 – the class for
23 those with the most severe and limiting impairments - were able to complete the majority of tests in
24 the test battery. One of the major limitations of the study was that the Para swimmers did not

1 complete the supported prone position assessments of shoulder ROM (shoulder extension,
2 horizontal abduction and unilateral flexion) due to time constraints and limited personnel. These
3 data were collected during training camps so, unfortunately, it was inevitable that some measures
4 could not be taken. As such, it is not yet known whether these supported prone positions are easily
5 administered in swimming athletes with a disability or whether these measures produce systematic
6 differences in ROM between non-disabled participants and swimming athletes with a disability.
7 Additionally, as can be seen with the large ICC 95% confidence intervals for some measures
8 (Tables 2 and 3), the sample size for the reliability measures is smaller than ideal to provide
9 meaningful minimum detectable changes (Lexell & Downham, 2005) although the sample used for
10 the respective reliability measures (intra- and inter-examiner) were very similar to those that have
11 previously assessed the reliability of shoulder ROM (Bak & Magnusson, 1997; Furness, et al.,
12 2015; Walker, et al., 2016). A further limitation was that inclinometer measurements of knee
13 flexion and elbow ROM were only included for inter-examiner testing. Additionally, as this test
14 battery focused on the assessment of motions relevant to S-class swimming, it is likely that
15 additional tests addressing hip ~~external~~-rotation, ankle dorsi-flexion and ~~forearm-ankle~~ supination
16 are required for accurate SB-class (breaststroke) classification. Finally, although these tests were
17 found to be reliable in a non-disabled population, reliability is a population specific characteristic,
18 therefore the reliability of these tests needs to be confirmed in a disabled population before their
19 utility in the classification process is established.

20 Conclusion

21 Overall, the novel ROM tests assessed for this study had good to excellent intra-examiner and inter-
22 examiner reliability in non-disabled participants. In addition to evaluating the reliability for these
23 ROM measures, preliminary normative ROM values for both non-disabled participants and Para
24 swimmers have also been established. Finally, this study identified that Para swimmers had

- 1 significantly less ROM than non-disabled participants. Further research should focus on the
- 2 reliability of these tests in Para swimmers and this test battery should be validated against
- 3 swimming performance in both abled-bodied and Para swimmers to determine which tests or
- 4 combination of tests best predict swimming performance.

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Table 1: Characteristics of non-disabled participants and Para swimmers

	Non-disabled	Swimmers with hypertonia	Swimmers with impaired muscle power
n	42	11	13
Health condition	N/A	CP (n=10), ABI (n=1)	SCI (n=12), polio (n=1),
Age (years)	23.2 (4.5)	27 (5.7)	30 (6.4)
Height (m)	1.74 (0.18)	1.66 (0.16)	1.62 (0.14)
Mass (kg)	73.5 (11.5)	66.6 (10.7)	60.5 (13.5)
BMI (kg/m²)	23.4 (2.9)	24.3 (3.6)	22.8 (2.6)

Values presented as mean (SD); BMI = body mass index; N/A = not applicable; CP = cerebral palsy; ABI = acquired brain injury; SCI = spinal cord injury

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Table 2: Intra-examiner reliability for ROM measures in non-disabled participants

Measure	ICC	ICC 95% CI	SEM	T test p value
Bilateral Shoulder flexion ^(I)	0.95	0.86-0.98	2.96	0.39
Bilateral Shoulder abduction ^(I)	0.73	0.24-0.91	3.85	0.22
Elbow flexion L ^(G)	0.82	0.48-0.94	1.69	0.19
Elbow flexion R ^(G)	0.81	0.46-0.94	1.56	0.40
Elbow extension L ^(G)	0.95	0.84-0.98	1.84	0.04
Elbow extension R ^(G)	0.94	0.81-0.98	1.42	0.95
Lower-limb streamline thigh L ^(I)	0.91	0.75-0.97	1.18	0.51
Lower-limb streamline thigh R ^(I)	0.83	0.51-0.94	1.80	0.25
Lower-limb streamline shank L ^(I)	0.89	0.69-0.96	1.31	0.63
Lower-limb streamline shank R ^(I)	0.91	0.71-0.97	1.26	0.87
Lower-limb streamline L knee ^(I)	0.94	0.82-0.98	1.40	0.31
Lower-limb streamline R knee ^(I)	0.91	0.75-0.97	1.61	0.26
Lower-limb streamline L ankle plantar-flexion ^(I)	0.95	0.57-0.99	1.67	≤0.01
Lower-limb streamline R ankle plantar-flexion ^(I)	0.96	0.89-0.99	1.73	0.22
Hip flexion L ^(I)	0.95	0.85-0.98	2.91	0.65
Hip flexion R ^(I)	0.92	0.76-0.97	3.45	0.24
Knee flexion L ^(G)	0.95	0.81-0.98	1.33	0.04
Knee flexion R ^(G)	0.88	0.64-0.96	2.64	0.38
Shoulder internal rotation L ^(I)	0.91	0.72-0.97	3.48	0.83
Shoulder internal rotation R ^(I)	0.88	0.64-0.96	4.00	0.61
Shoulder external rotation L ^(I)	0.83	0.48-0.94	6.11	0.56
Shoulder external rotation R ^(I)	0.81	0.43-0.94	6.29	0.91
Prone shoulder horizontal abduction L ^(I)	0.87	0.62-0.96	3.07	0.56
Prone shoulder horizontal abduction R ^(I)	0.82	0.48-0.94	3.26	0.14
Prone shoulder extension, elbow flexed L ^(I)	0.94	0.82-0.98	3.09	0.70
Prone shoulder extension, elbow flexed R ^(I)	0.90	0.68-0.97	3.95	0.17
Prone shoulder extension, elbow extended L ^(I)	0.94	0.82-0.98	3.46	0.31
Prone shoulder extension, elbow extended R ^(I)	0.90	0.71-0.97	4.60	0.79
Prone shoulder flexion L ^(I)	0.96	0.87-0.99	2.37	0.15
Prone shoulder flexion R ^(I)	0.90	0.71-0.97	3.61	0.80
Functional reach Forwards ^(T)	0.66	-0.02-0.89	2.24	0.48
Functional reach L ^(T)	0.80	0.41-0.93	2.00	0.31
Functional reach R ^(T)	0.68	0.07-0.89	2.35	0.31

Functional reach backwards ^(I) 0.94 0.83-0.98 2.51 0.37

L = left; R = right; ^(I) = measurement with inclinometer; ^(G) = measurement with goniometer; ^(T) = measurement with tape measure; ICC = intraclass correlation coefficient; ICC 95% CI = intraclass correlation coefficient 95% confidence intervals; SEM = standard error of measurement; T test conducted on mean values from session one and two.

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Table 3: Inter-examiner reliability for ROM measures in non-disabled participants

Measure	ICC	ICC 95% CI	SEM	T-test p value
Bilateral Shoulder flexion ⁽¹⁾	0.98	0.94-0.99	1.42	0.99
Bilateral Shoulder abduction ⁽¹⁾	0.85	0.59-0.95	2.74	0.20
Elbow flexion L ^(G)	0.79	0.17-0.94	2.04	≤0.01
Elbow flexion R ^(G)	0.67	0.10-0.88	3.05	0.03
Elbow extension L ^(G)	0.76	0.30-0.92	1.88	0.03
Elbow extension R ^(G)	0.73	0.17-0.91	2.12	0.01
Elbow flexion L ⁽¹⁾	0.82	0.13-0.95	3.81	≤0.01
Elbow flexion R ⁽¹⁾	0.86	0.61-0.95	3.79	0.18
Elbow extension L ⁽¹⁾	0.90	0.70-0.97	3.19	0.09
Elbow extension R ⁽¹⁾	0.75	0.26-0.91	3.94	0.93
Lower-limb streamline thigh L ⁽¹⁾	0.92	0.77-0.97	1.10	0.17
Lower-limb streamline thigh R ⁽¹⁾	0.92	0.77-0.97	0.73	0.55
Lower-limb streamline shank L ⁽¹⁾	0.89	0.67-0.96	1.44	0.76
Lower-limb streamline shank R ⁽¹⁾	0.80	0.42-0.93	1.77	0.50
Lower-limb streamline L knee ⁽¹⁾	0.88	0.68-0.96	0.88	0.31
Lower-limb streamline R knee ⁽¹⁾	0.79	0.41-0.93	0.79	0.41
Lower-limb streamline L ankle plantar-flexion ⁽¹⁾	0.98	0.94-0.99	0.98	0.65
Lower-limb streamline R ankle plantar-flexion ⁽¹⁾	0.98	0.95-0.99	0.98	0.84
Hip flexion L ⁽¹⁾	0.88	0.57-0.96	3.14	0.02
Hip flexion R ⁽¹⁾	0.92	0.76-0.97	2.40	0.70
Knee flexion L ^(G)	0.21	-0.71-0.69	3.50	0.04
Knee flexion R ^(G)	0.72	0.23-0.90	2.43	0.26
Knee flexion L ⁽¹⁾	0.85	0.55-0.95	3.09	0.97
Knee flexion R ⁽¹⁾	0.82	0.48-0.94	3.51	0.52
Shoulder internal rotation L ⁽¹⁾	0.86	0.42-0.96	6.52	0.01
Shoulder internal rotation R ⁽¹⁾	0.86	0.50-0.95	6.34	0.02
Shoulder external rotation L ⁽¹⁾	0.92	0.78-0.97	4.96	0.13
Shoulder external rotation R ⁽¹⁾	0.95	0.85-0.98	4.22	0.97
Supported internal rotation L ⁽¹⁾	0.81	0.45-0.94	5.73	0.95
Supported internal rotation R ⁽¹⁾	0.90	0.71-0.97	3.80	0.60
Prone shoulder horizontal abduction L ⁽¹⁾	0.93	0.79-0.97	3.85	0.91
Prone shoulder horizontal abduction R ⁽¹⁾	0.86	0.62-0.95	4.80	0.31
Prone shoulder extension, elbow flexed L ⁽¹⁾	0.96	0.89-0.99	2.75	0.93
Prone shoulder extension, elbow flexed R ⁽¹⁾	0.95	0.87-0.98	2.79	0.05
Prone shoulder extension, elbow extended L ⁽¹⁾	0.96	0.88-0.99	2.99	0.61
Prone shoulder extension, elbow extended R ⁽¹⁾	0.96	0.88-0.99	2.65	0.61
Prone shoulder flexion L ⁽¹⁾	0.84	0.55-0.94	3.36	0.40

Prone shoulder flexion R ^(I)	0.95	0.85-0.98	2.24	0.80
Functional reach forwards ^(T)	0.73	0.21-0.91	2.74	0.75
Functional reach L ^(T)	0.76	0.29-0.92	2.45	0.11
Functional reach R ^(T)	0.62	0.02-0.86	2.96	0.94
Functional reach backwards ^(T)	0.92	0.76-0.92	2.24	0.08

L = left; R = right; ^(I) = measurement with inclinometer; ^(G) = measurement with goniometer; ^(T) = measurement with tape measure; ICC = intraclass correlation coefficient; ICC 95% CI = intraclass correlation coefficient 95% confidence intervals; SEM = standard error of measurement; T test conducted on mean values from examiner one and two.

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Table 4: Range of motion preliminary normative values for entire test battery for non-disabled participants and Para swimmers

Measure	Non-disabled ROM degrees (SD)	Swimmers with Hypertonia ROM degrees (SD)	Swimmers with impaired muscle power ROM degrees (SD)
Bilateral Shoulder flexion ⁽¹⁾	165 (12)	151 (15)	147 (31)
^β Bilateral Shoulder abduction ⁽¹⁾	184 (8)	186 (12)	179 (20)
Elbow flexion L ^(G)	143 (5)	135 (7)	132**(21)
Elbow flexion R ^(G)	144 (6)	136 (8)	128**(33)
Elbow extension L ^(G)	-1.4 (6)	-11** (12)	-8.4* (8)
Elbow extension R ^(G)	-2.3 (6)	-6.6 (8)	-8.0* (9)
Elbow flexion left ⁽¹⁾	146 (9)		
Elbow flexion right ⁽¹⁾	146 (11)		
Elbow extension left ⁽¹⁾	4.7 (9)		
Elbow extension right ⁽¹⁾	4.8 (11)		
Elbow total ROM left ⁽¹⁾	151 (17)		
Elbow total ROM right ⁽¹⁾	151 (15)		
^β Lower-limb streamline thigh L ⁽¹⁾	8.1 (7)	2.0 (10)	3.7 (17)
^β Lower-limb streamline thigh R ⁽¹⁾	6.7 (6)	0.9 (11)	2.0 (18)
^β Lower-limb streamline shank L ⁽¹⁾	5.3 (5)	-16** (13)	-15** (20)
^β Lower-limb streamline shank R ⁽¹⁾	5.4 (6)	-13** (11)	-14** (20)
^β Lower-limb streamline L knee ⁽¹⁾	2.8 (6)	18* (22)	19* (37)
^β Lower-limb streamline R knee ⁽¹⁾	1.3 (5)	14 (22)	15 (38)
^β Lower-limb streamline L ankle plantar-flexion ⁽¹⁾	9.5 (10)	40** (19)	33** (12)
^β Lower-limb streamline R ankle plantar-flexion ⁽¹⁾	7.9 (10)	38** (21)	33** (16)
Hip flexion L ⁽¹⁾	119 (13)	69** (32)	44** (54)
Hip flexion R ⁽¹⁾	118 (13)	67**^ (31)	36** (46)
Knee flexion L ^(G)	135 (7)	100**^ (34)	59 ** (63)
Knee flexion R ^(G)	134 (8)	101**^ (27)	54** (64)
Knee flexion L ⁽¹⁾	36 (8)		
Knee flexion R ⁽¹⁾	37 (8)		
Shoulder internal rotation L ⁽¹⁾	83 (17)	36**^ (19)	56** (13)
Shoulder internal rotation R ⁽¹⁾	78 (16)	44** (17)	55** (13)
Shoulder external rotation L ⁽¹⁾	92 (15)	82 (18)	77* (25)
Shoulder external rotation R ⁽¹⁾	97 (15)	88 (11)	85 (20)
^β Shoulder internal rotation supported L ⁽¹⁾	89 (11)		
^β Shoulder internal rotation supported R ⁽¹⁾	84 (10)		
^β Prone shoulder horizontal abduction L ⁽¹⁾	31 (12)		
^β Prone shoulder horizontal abduction R ⁽¹⁾	32 (12)		

β Prone shoulder extension, elbow flexed L ^(I)	44 (14)		
β Prone shoulder extension, elbow flexed R ^(I)	46 (14)		
Prone shoulder extension, elbow extended L ^(I)	33 (16)		
Prone shoulder extension, elbow extended R ^(I)	35 (14)		
β Prone shoulder flexion L ^(I)	169 (12)		
β Prone shoulder flexion R ^(I)	167 (12)		
β Functional reach forwards ^(T)	54 (7)	42* [^] (11)	15** (20)
β Functional reach L ^(T)	23 (5)	15** [^] (4)	7.9** (10)
β Functional reach R ^(T)	24 (5)	15** [^] (3)	8.0** (9)
β Functional reach backwards ^(T)	35 (10)	17** [^] (5)	6.9** (9)

Values presented as mean (SD) for degrees of range of motion or distance (cm) for functional reach measures. L = left; R = right; ^(I) = measurement with inclinometer; ^(G) = measurement with goniometer; ^(T) = measurement with tape measure; *significantly different to non-disabled participants ($p \leq 0.05$); ** significantly different to non-disabled participants ($p \leq 0.01$); [^] significantly different from athletes with impaired muscle power ($p \leq 0.05$). β designate novel tests that are not in the current classification system (all tests are described in supplementary table 1). Area in grey represents tests that were not completed by Para swimmers due to time/personnel restrictions.

